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On the Low Frequency Noise in Ion Sensing

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Abstract

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Ion sensing represents a grand research challenge. It finds a vast variety of applications in, e.g., gas sensing for domestic gases and ion detection in electrolytes for chemical-biological-medical monitoring. Semiconductor genome sequencing exemplifies a revolutionary application of the latter. For such sensing applications, the signal mostly spans in the low frequency regime. Therefore, low-frequency noise (LFN) present in the same frequency domain places a limit on the minimum detectable variation of the sensing signal and constitutes a major research and development objective of ion sensing devices. This thesis focuses on understanding LFN in ion sensing based on both experimental and theoretical studies.

The thesis starts with demonstrating a novel device concept, i.e., ion-gated bipolar amplifier (IGBA), aiming at boosting the signal for mitigating the interference by external noise. An IGBA device consists of a modified ion-sensitive field-effect transistors (ISFET) intimately integrated with a bipolar junction transistor as the internal current amplifier with an achieved internal amplification of 70. The efficacy of IGBA in suppressing the external interference is clearly demonstrated by comparing its noise performance to that of the ISFET counterpart.

Among the various noise sources of an ISFET, the solid/liquid interfacial noise is poorly studied. A differential microelectrode cell is developed for characterizing this noise component by employing potentiometry and electrochemical impedance spectroscopy. With the cell, the measured noise of the TiN/electrolyte interface is found to be of thermal nature. The interfacial noise is further found to be comparable or larger than that of the state-of-the-art MOSFETs. Therefore, its influence cannot be overlooked for design of future ion sensors.

To understand the solid/liquid interfacial noise, an electrochemical impedance model is developed based on the dynamic site-binding reactions of surface hydrogen ions with surface OH groups. The model incorporates both thermodynamic and kinetic properties of the binding reactions. By considering the distributed nature of the reaction energy barriers, the model can interpret the interfacial impedance with a constant-phase-element behavior. Since the model directly correlates the interfacial noise to the properties of the sensing surface, the dependencies of noise on the reaction rate constants and binding site density are systematically investigated.

Keywords: low frequency noise, ion sensor, ISFET, electrochemical impedance spectroscopy, constant phase element, surface chemistry, CMOS technology

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List of Papers

This thesis is based on the following papers, which are referred to in the text by their Roman numerals.

- I Zhang, D. Gao X., Chen S., Norström H., Smith U., Solomon P., Zhang S.L., Zhang Z. (2008) An ion-gated bipolar amplifier for ion sensing with enhanced signal and improved noise performance. *Applied Physics Letters*, 105(8):802102
- II Zhang D., Must I., Netzer N.L., Xu X., Solomon P., Zhang S.L., Zhang Z. (2016) Direct assessment of solid-liquid interface noise in ion sensing using a differential method. *Applied Physics Letters*, 108(15), 151603
- III Zhang D., Solomon P., Zhang S.L., Zhang Z (2017) Low-frequency noise originating from the dynamic hydrogen ion reactivity at the solid/liquid interface of ion sensors. *Sensors and Actuators B*, submitted
- IV Zhang D., Solomon P., Zhang S.L., Zhang Z (2017) Correlation of Low-Frequency Noise to the Dynamic Properties of the Sensing Surface in Electrolytes. *ACS sensors*, Submitted

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Author's Contributions

- I Minor part of planning and the device fabrication, all of the TCAD simulation and measurement, and most of the data analysis and the writing.
- II Major part of planning, all of the device design and fabrication, EIS measurement and SEM, most of the data analysis, and all of the writing.
- III Major part of planning, most of the model development, and all of the measurement, the data analysis and the writing.
- IV All of the planning, most of the data analysis, and all of the writing.

Table of Contents

1. Introduction	13
1.1. Background	13
1.1.1 ISFET technology	13
1.1.2. Noise sources in ISFET systems	
1.2. Research objectives	
1.3. Thesis organization	
2. Fundamentals	20
2.1. Sensing signal of ISFETs	20
2.1.1. Electrical double layer	20
2.1.2. Site-binding model and signal of ISFET	
2.2. Thermal noise in ion-sensing systems	
2.2.1. Fluctuation-dissipation theorem	23
2.2.2. Electrochemical impedance spectroscopy	
2.2.3. Constant phase element and 1/f noise	
3. Enhance SNR via Internal Amplification	27
3.1. Internal signal amplification	
3.2. Integration of internal current amplifier	29
3.3. DC Measurement of IGBA	31
3.4. SNR Enhancement via IGBA	32
3.4.1. Characterization details	32
3.4.2. Results and discussion	32
4. Assessment of Solid/Liquid Interface Noise in Ion-Sensing	35
4.1. Differential microelectrode cell	
4.1.1. Differential electrode configuration	35
4.1.2. Fabrication of the differential microelectrode cell	36
4.2. Measurement methods	37
4.2.1. Potentiometric noise	37
4.2.2. Thermal noise	38
4.3. Result and discussion	38
4.3.1. $1/f^{\gamma}$ nature of oxide/electrolyte interfacial noise	38
4.3.2. Significant extrinsic noise in ISFETs	
5. Electrochemical Impedance Modelling for Solid/Liquid Interface	42
5.1. Model development	

5.1.1 Interfacial impedance based on site-binding reactions	42
5.1.2 Variability in surface properties	43
5.2. Application of the proposed impedance model	
5.2.1 Experimental procedure and parameter extraction	45
5.2.2. <i>K</i> -distribution vs <i>c</i> -distribution	46
6. Understanding Oxide/Electrolyte Interface Noise	49
6.1. Noise modeling analysis	49
6.1.1. Parameter extraction	49
6.1.2. Noise dependence on the site-binding admittance	50
6.1.3. Averaging of distributed interfacial properties	52
6.2. Correlation of LFN to surface dynamic properties	53
6.2.1. Effect of reaction rate constant	
6.2.2. Effect of site density	55
6.2.3. Summarized remarks	55
7. Concluding Remarks and Future Perspective	57
Summary of the Appended Papers	59
Sammanfattning på svenska	61
Acknowledgement	64
Reference	66

Abbreviations and Symbols

ALD Atomic layer deposition BJT Bipolar junction transistor

CE Counter electrode

CMOS Complementary metal oxide semiconductor

CPE Constant phase element EDL Electrical double layer

EIS Electrochemical impedance spectroscopy

dNTP Deoxynucleoside triphosphate

EG Extended gate

GCS Gouy-Chapman-Stern HGP Human genome project IGBA Ion-gated bipolar amplifier

ISFET Ion-sensitive field-effect transistor

J-N Johnson- Nyquist

LDMOS Laterally diffused metal oxide semiconductor

LFN Low-frequency noise LPCVD chemical vapor deposition

MOSFET Metal oxide semiconductor field-effect transistor

NGS Next-generation sequencing

OCV Open-circuit voltage **PCR** Polymerase chain reaction **PDMS** polydimethylsiloxane **PSD** Power spectrum density **PZC** Point of zero charge RE Reference electrode RIE Reactive ion etching RMS Root-mean-square

SEM Scanning electron microscope

SBM Site-binding model

SMU Source and measurement unit

SNR Signal-to-noise ratio
TEOS Tetraethyl orthosilicate
WE Working electrode

 $a_{\rm S}$ Surface hydrogen ion concentration

 C_{buff} Buffer capacitance

 $C_{\rm DL}$ Electrical double layer capacitance

 C_{diff} Diffuse layer capacitance

 C_{Stern} Electrical double layer capacitance $c_{\text{A}}(c_{\text{B}})$ Reaction rate constant of protonation

 $c_{A0}(c_{B0})$ $c_{A}(c_{B})$ at energy center

 $E_{\rm A}^{\rm ad}(E_{\rm B}^{\rm ad})$ Activation energy for protonation reaction

 E_c Distributed kinetic energy barrier E_K Distributed Gibbs energy change

 $f_{\rm c}$ Corner frequency

 $f_{\rm M}$ Measurement frequency $\Delta G_{\rm A}(\Delta G_{\rm B})$ Gibbs energy change

 $g_{mD}(g_{mC})$ Transconductance of ISFET(IGBA)

 $I_{\rm B}$ Base current $I_{\rm C}$ Collector current $I_{\rm D}$ Drain current $I_{\rm E}$ Emitter current $I_{\rm S}$ Source current

*i*_D Internal current noise of ISFET

 $i_{\rm n}$ Input current noise of readout circuitry

 $K_{A}(K_{B})$ Equilibrium constant $K_{A0}(K_{B0})$ $K_{A}(K_{B})$ at energy center N_{S} Density of surface OH group

 $N_{\rm SS}$ $N_{\rm S}$ per unit energy

 pH_S Surface pH

 $R_{\rm b}$ Liquid bulk resistance

 $r_{\rm A}(r_{\rm B})$ Reaction rate constant of deprotonation

 S_{pH} pH sensitivity S_{V} Noise PSD

 $S_{\rm V}^{\rm pot}$ Potentiometric noise PSD $S_{\rm V}^{\rm th}$ Thermal noise PSD

SNR in Internal SNR

 SNR_{α}^{ex} External SNR without internal amplification SNR_{α}^{ex} External SNR with internal amplification

 $V_{\rm D}$ Drain voltage $V_{\rm E}$ Emitter voltage $V_{\rm G}$ Gate voltage

 $V_{\rm T}$ Threshhold voltage

 $v_{\rm n}$ Input voltage noise of readout circuitry

 Y_{SB} Site-binding admittance y_{SB} Y_{SB} per unit energy

 Z_{CPE} Impedance spectrum of a CPE Z_{int} Solid/liquid interfacial impedance

 Z_{SB} Site-binding impedance β Current amplification of BJT

$oldsymbol{eta_{ ext{int}}}$	Intrinsic buffer capacity
Θ_+	Fraction of positively charged OH group
Θ_	Fraction of negatively charged OH group
Θ_0	Fraction of neutral OH group
$oldsymbol{\sigma}_0$	Surface charge density
$\sigma_c(\sigma_{\scriptscriptstyle K})$	Standard deviation of energy distribution
φ_0	Surface potential

1. Introduction

Noise is a stochastic process, appearing spontaneously as random time and/or space series of dynamic variables of interest [1]. Elimination of noise is impossible, because any substrate is subjected to thermal fluctuation, as long as the temperature is above 0 K. This thesis will look into this ubiquitous and everlasting phenomena present in ion-sensing applications. In Section 1.1, let's use an example of ion-sensing applied in cutting edge technology to demonstrate the importance of addressing noise in the ion-sensing applications, which motivates the research objects of the thesis in Section 1.2 and thesis organization in Section 1.3.

1.1. Background

1.1.1. ISFET technology

Human genome project (HGP) [2], genechips [3], personalized molecular diagnosis [4], etc., all such eye-catching concepts in life science and research are closely linked to a field – genome sequencing, the process of finding out the precise sequence of the four nucleotide base pairs in a DNA molecule. A DNA molecule comprises genes that bear the complete genetic information of a living organism. Therefore, accurate acquisition of the genetic information of the organism always has tremendous significance for the study of life science. The genome sequencing establishes a valuable method that guides people to find genes much more easily and quickly, which becomes an important progress towards understanding the complexity and diversity of lives.

Generally, the genome sequencing refers to any method or technology that can be used to determine the sequence of the bases. Based on the selective incorporation of chain-terminating dideoxynucleotides by DNA polymerase chain reaction (PCR) [5], [6], the Sanger sequencing method was developed in 1977 [5], prevailing approximately from the 1980s until the mid-2000s. However, the Sanger method is tremendously costly and time-inefficient. Initiated in 1990, the HGP based on the Sanger method consumed 2.7 billion dollars when it was declared complete in 2003 [7]. In the next decade, however, revolutionary technological advances reached the sequencing market [8]–[12], leading to much more efficient sequencing at

lower costs. The human genome can be sequenced within one day, at a cost of as low as around \$1,000 in 2015 [13]. The emergence of fast and affordable DNA sequencing is an important step towards personalized medicine, and revolutionized genomics and molecular biology.

Featured with high-throughput parallel sequencing, the set of the modern advanced sequencing technologies is collectively referred to as nextgeneration sequencing (NGS) [8], [9]. Among various cutting-edge approaches, the ion-semiconductor, or Ion Torrent, sequencing technology [16] is one of the important players in the NGS arena, owing to its rapid and costeffective test method[17], as well as its system-level integration using complementary metal oxide semiconductor (CMOS) technology. As shown in Figure 1(a), the Ion Torrent sequencing system is integrated as a bench-top platform, and its core component is a disposable sequencing chip, illustrated in Figure 1(b). On each sequencing chip, millions of microwells are fabricated, and each well contains a bead that bears over 10,000 replications of a single-stranded DNA template to be sequenced, as illustrated in Figure 1(c). During a sequencing process, the wells are sequentially flooded with A, C, G or T deoxynucleoside triphosphate (dNTP).[18]-[20] If the incoming dNTP is complementary to the next unpaired base on the DNA template, the dNTP molecule reacts with the nucleotide on each DNA strand to form a base pair, releasing a hydrogen ion (H⁺).

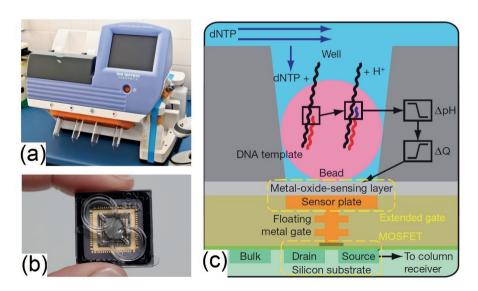


Figure 1. (a) Ion Torrent bench-top DNA sequencing platform, and its (b) Sequencing chip. (c) The schematic cross-section of an ISFET fabricated on the sequencing chip as a pH sensor, by courtesy of J.M. Rothberg el.[16] On top of it is the liquid well where an acrylamide bead is placed to bear the DNA template.

Therefore, thousands of H^+ released from the DNA replications decreases the local pH in the well, and the pH change is then detected by a metal-oxide-sensing gate beneath the well that is connected to the metal gate of a metal oxide field effect transistor (MOSFET), as marked in *Figure 1*(c). The MOSFET with an extended sensing gate is also called extended-gated ion sensitive field effect transistor (EG-ISFET)[21]–[23].

To understand the working principle of an ISFET, it is instructive to understand the operation of its archetype configuration: a MOSFET. A typical MOSFET has three terminals, known as source, drain and gate, as depicted in *Figure 2*(a), i). The voltage V_G applied to the gate can modulate the resistance between the source (**S**) and the drain (**D**), and hence the current I_D flowing between them, provided that a certain voltage V_{DS} is applied between the source and drain. This I_D - V_G relation of an MOSFET, schematically depicted in *Figure 2*(a), ii), is also known as transfer characteristics of the MOSFET. As seen in the figure, I_D "turns on" as V_G goes beyond a certain knee point voltage denoted with V_T . The corresponding theories have been extensively detailed in standard textbooks [24].

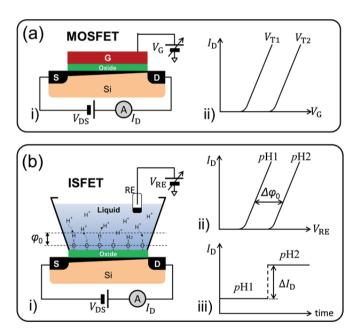


Figure 2. i) Cross-sectional sketches and ii) typical transfer characteristics of (a) a MOSFT and (b) an ISFET. The transfer characteristics are depicted with two distinct $V_{\rm T}$ for the MOSFET, while with two pH values for the ISFET. At certain $V_{\rm RE}$, $\Delta I_{\rm D}$ caused by changing pH for the ISFET is schematically depicted in iii) as well.

As to an ISEFT, a more general configuration than those with extended gates is illustrated in *Figure 2*(b), i), in which the solid metal gate of a MOSFET is replaced by a liquid under test. To operate the ISFET, a reference electrode

is submerged in the liquid and biased with $V_{\rm RE}$ to anchor the electrochemical potential of the liquid. Therefore, $I_{\rm D}$ - $V_{\rm RE}$ relation represents the transfer characteristics of the ISFET. As $p{\rm H}$ of the liquid varies, to maintain surface equilibrium, amphoteric hydroxyl (OH) groups on the oxide surface can capture/release ${\rm H}^+$, accordingly, resulting in surface charge variation. Thus, the oxide surface electric potential φ_0 with respect to the liquid bulk will change, modulating the resistance between ${\bf S}$ and ${\bf D}$ and then causing a change in $I_{\rm D}$. Therefore, the transfer curve shifts as the $p{\rm H}$ value changes, as illustrated in $Figure\ 2({\rm b})$, ii). $\Delta I_{\rm D}$ caused by $\Delta p{\rm H}$ at a certain $V_{\rm RE}$ is referred to as the signal of the ISFET. The quantification of $\varphi_0 - p{\rm H}$ relation becomes a crucial concern for understanding the operation principle of an ISFET, which has been well addressed by the site-binding model (SBM) and will be briefly discussed in next section.

The ISFET applied in Ion Torrent technology is fabricated with the standard CMOS technology, granting it another significant advantage: the ability to scale with Moore's Law. Moore's law, based on the observed trend over the past decades, states that roughly every two years the amount of transistors in a single integrated circuit chip doubles, leading to more high-performance chips with denser packages. It means that the throughput of the Ion Torrent sequencing system can be brought even higher, with a denser ISFET array, which is readily achieved by scaling down the ISFET's sizes via the CMOS technology [25].

However, ultra-scale integration of ISFET is not always beneficial, in terms of the noise performance of the ISFET. As *Figure 3*[16] shows, notable fluctuation appears at the signal baseline (0 count), as the diameter of the liquid well on top of the ISFET decreases, which may be caused by various mechanisms, such as the higher potential noise with smaller sensing gate area, and boosted cross-talk from the denser integration, etc.

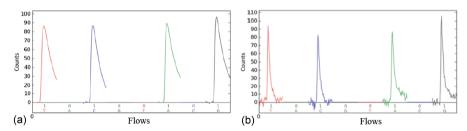


Figure 3. Sequencing signal (measured in the voltage counts) v.s. base flow for the Ion Torrent sequencer from (a) 3.5 μ m diameter well and (b) 1.3 μ m well of its ISFETs, by courtesy of J.M. Rothberg el.[16] Note the larger fluctuation at the signal base for the smaller size.

Since complete elimination of the noise is impossible, in any sensing system, the noise will ultimately determine the sensing resolution, by placing a limit on the minimum detectable variation of signal. For sensing applications like

Ion Torrent sequencing, a single base incorporation leads to a 0.02 pH variation [16], corresponding to around 1 mV change in the surface potential provided the Nernst response applies. To measure such a small potential change, the noise in the sensing system must be mitigated to an appreciable extend.

1.1.2. Noise sources in ISFET systems

The major contribution to the noise in ion-sensing applications dominates in the low-frequency regime, where sensing experiments are typically performed [26]. Besides, heavy metallization in sensing chips is subject to low frequency noise coupling which can interfere with biomedical signals that mostly span in the same frequency domain [27]. Hence, low-frequency noise (LFN) becomes an significant performance-limiting factor for ion-/biosensitive FET systems, which has thus received extensive in-depth investigations [26], [28]–[46]. The noise sources of an ISFET system are sorted out as follows.

In an ISFET-based ion sensing system, any noise sources outside the ISFET itself are referred to as the external noise, such as environmental interference and instrument noise from terminal read-out circuits [47] etc., as illustrated in *Figure 4*. It can be demanding or even impossible to mitigate the external noise, but their interference can be diminished by internally amplifying the signals, as will be discussed in next chapter,

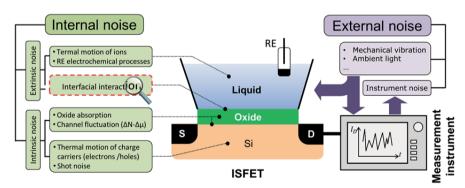


Figure 4. Noise sources appearing in an ion sensing system consisting of an ISFET and characterization instrument. The noise associated with the solid/liquid interfacial interaction is a research focus of this thesis.

Noise present inside an ISFET is referred to as the internal noise of the ISFET, falling into intrinsic and extrinsic parts, which is also illustrated in *Figure 4*. The intrinsic noise refers to that appearing in the solid part of an ISFET. It consists of, among other possible sources, the channel noise [28], [30]–[32], [36], [38], [41], [43] caused by fluctuation of the carrier number (ΔN) and/or mobility $(\Delta \mu)$, the thermal noise associated with the dielectric

absorption [40], [42], the shot noise arising from the electrical potential barrier [48], and thermal noise associated with the contact resistance of the source and drain terminals [33]. On the other hand, the noise of an ISFET can also originate from the liquid part of the ISFET, referred to as extrinsic noise of the ISFET. The extrinsic noise is generally rooted in ionic interaction at the liquid/oxide interface [26], [37], [39], [44], [46], electrochemical process between liquid and RE [29], as well as thermal noise from the liquid bulk.

The theoretical and experimental concerns behind the intrinsic noise sources have been well understood in the literatures. The extrinsic noise originates from the RE and liquid bulk can be accounted for by well-established models [29], owing to the simplicity of the associated electrochemical process. The major challenge of addressing the noise of the ISFET lies in understanding the solid/liquid interfacial noise.

1.2. Research objectives

This thesis work aims at a systematic investigation of the LFN present in the field-effect ion sensing systems, and, in particular, understanding the noise originating from the solid/liquid interface where the signal to be detected is generated and the corresponding sensing mechanisms are sought for. First, to diminish the external interference, technology of the internal amplification needs to be explored. Second, one major challenge is to accurately assess the solid/liquid interfacial noise, which motivates a dedicated characterization tool. Last, understanding the noise significantly relies on a theoretical model that incorporates the physical properties of the solid/liquid interface, in order to establish the relationship between the noise and such properties.

In terms of the above experimental and theoretical concerns, the tasks of the thesis are summarized as

- to design and fabricate the dedicated device for internal amplification.
- to design and fabricate the dedicated device for the solid/liquid interfacial noise study,
- to develop a theoretical model that links the interfacial noise to the physical properties of the interface, and
- to utilize the model to interpret the noise behavior, as well as its dependence on the interface properties.

1.3. Thesis organization

The thesis is structured as follows:

Chapter 2 introduces the electrical double layer (EDL) structure as well as SBM for explaining the pH-sensing principle of the ISFET, as well as the theoretical background of the thermal noise present in ion-sensing.

Chapter 3 demonstrates the novel device concept towards signal-to-noise ratio (SNR) enhancement for the ISFET systems by suppressing the interference from the external noise. The conceptualized internal amplification, as the operation principles of the device, is described. The CMOS technology-based fabrication flow for the device is detailed as well. The DC and noise spectrum characterizations of the device are shown to indicate its efficacy of achieving greater SNR.

Chapter 4 introduces a differential microelectrode array dedicated for characterizing the solid/liquid interfacial noise. The working principle of the differential measurement and the fabrication details are described. The noise measurement setups based on potentiometry and electrochemical impedance spectroscopy for the electrode cell are described, and the measurement results are summarized and discussed.

In Chapter 5, an electrochemical impedance model, based on the hydrogen ion reactivity at the oxide/electrolyte interface, is developed for studying the physical mechanism behind the interfacial noise. The modeling method is detailed, and the validity of the model is justified through the extracted modeling parameters.

In Chapter 6, the proposed impedance model is explored in detail, in order to find out the dependence of the interfacial noise on the surface dynamic properties.

The thesis is concluded in Chapter 7 with a general summary and a future outlook. In Chapter 8 an overview of the appended papers is provided.

2. Fundamentals

Noise can be rooted in variety of mechanisms. From the standpoint of electronic ion sensing, the noise refers to the unwanted fluctuation superimposed on an electrical signal. In this chapter, the fundamentals pertaining to the noise present in electronic sensing systems, particularly ISFET, are briefly reviewed. In section 2.1, the structure of electric double layer (EDL) as well as site-binding model (SBM) will be discussed firstly, in order to quantify the ISFET signal. Then, the basics and characterization of thermal noise will be discussed in section 2.2.

2.1. Sensing signal of ISFETs

2.1.1. Electrical double layer

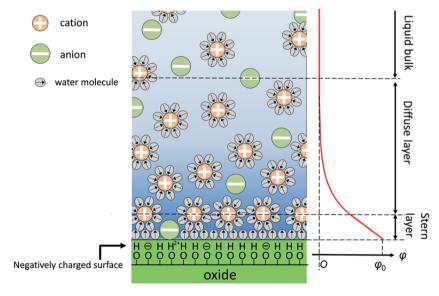


Figure 5. Schematic of an EDL at the interface between a negatively charged oxide and and electrolyte. The distribution of electrical potential φ from the oxide surface to the liquid bulk is also illustrated.

When a solid electrode is brought in contact with a liquid, two spatially separated charge layers from the liquid will appear on top of the electrode sur-

face, referred to as EDL. The EDL structure plays a fundamental role in the surface charging. Therefore, understanding the EDL structure at the oxide/electrolyte interface is import for understanding the corresponding charging mechanism. Many EDL models have been applied successfully in their respective regard, in which the Gouy-Chapman-Stern (GCS) model has been extensively employed for ISFET applications [49]. In *Figure 5*, the EDL structure described with the GCS model is schematically depicted for a negatively-charged oxide in contact with an electrolyte. As shown in the figure, the first layer of the EDL, i.e. the Stern layer, consists of the solvated ions adsorbed onto the oxide surface due to chemical interactions [50]. The second layer, i.e. the diffuse layer, comprises the ions attracted electrostatically by the surface charge, loosely surrounding the oxide surface [50]. Then, the surface potential φ_0 is the potential drop across both layers, and the EDL capacitance C_{DL} is the series connection of the Stern capacitance C_{Stern} and the diffuse layer capacitance C_{diff} , as expressed with the following relation:

$$C_{\rm DI}^{-1} = C_{\rm Stern}^{-1} + C_{\rm diff}^{-1} \tag{2.1}$$

2.1.2. Site-binding model and signal of ISFET

The well-known Nernstian equation predicts that the variation of φ_s with one pH unit change of solution, also known as pH sensitivity, is 59.2 mV at room temperature. In the case of oxide/liquid systems, however, the observed pH sensitivity is generally less than 59 mV. To explain the deviation, the site-binding model [51], as well as its derivatives[52], [53], was developed to describe the charging for an oxide/liquid interface, which successfully interprets the observed non-Nernstian sensitivity and has been widely accepted as the primary charging mechanism of the oxide-liquid interfaces. In the context of SBM, the oxide charging is ascribed to the H^+ adsorption to/desorption from the amphoteric OH group, i.e. protonation/deprotonation, on the oxide surface, as summarized by the following reversible reactions:

$$M-OH \leftrightarrow M-O^- + H_S^+ \tag{2.2a}$$

$$M-OH_2^+ \leftrightarrow M-OH + H_S^+ \tag{2.2b}$$

where, H_s⁺ denotes the surface H⁺. In thermal equilibrium, the two reactions are equilibrated by the following detailed balances:

$$c_{\mathcal{A}} a_{\mathcal{S}} [\mathbf{M} \cdot \mathbf{O}^{-}] = r_{\mathcal{A}} [\mathbf{M} \cdot \mathbf{O} \mathbf{H}]$$
 (2.3a)

$$c_{\rm B}a_{\rm S}[{\rm M\text{-}OH}] = r_{\rm B}[{\rm M\text{-}OH}_2^+]$$
 (2.3b)

where, [M-O⁻], [M-OH₂⁺], and [M-OH] denote the density of deprotonated, protonated, and uncharged surface OH groups, respectively, and $a_{\rm S}$ the H_S⁺ concentration; c and r represent the reaction rate constant for the H⁺ adsorption and desorption, with subscripts A and B referring them to reactions (2.2a) and (2.2b), respectively. By definition, $c_{\rm A}$ and $c_{\rm B}$ are related to the kinetic barriers of the H⁺ adsorption $E_{\rm A}^{\rm ad}$ and $E_{\rm B}^{\rm ad}$ via:

$$c_{\rm A} = c_{\rm A}' \exp\left(-\frac{E_{\rm A}^{\rm ad}}{kT}\right), \ c_{\rm B} = c_{B}' \exp\left(-\frac{E_{\rm B}^{\rm ad}}{kT}\right)$$
 (2.4)

where c'_A and c'_B are constants, k is the Boltzmann constant, T the temperature. Likewise, r_A and r_B are functions of the kinetic energy of the H⁺ desorption, with the same form as c_A and c_B . Therefore, the surface equilibria can be characterized by two thermodynamic equilibrium constants as follows:

$$K_{\rm A} = \frac{r_{\rm A}}{c_{\rm A}} = K_{\rm A}' \exp\left(-\frac{\Delta G_{\rm A}}{kT}\right), \quad K_{\rm B} = \frac{r_{\rm B}}{c_{\rm B}} = K_{\rm B}' \exp\left(-\frac{\Delta G_{\rm B}}{kT}\right)$$
 (2.5)

in which, K_A' and K_B' are constants, and the two ΔG :s denote the Gibbs free energy changes for reactions (2.2a) and (2.2b), respectively. In practice, K_A and K_B are often featured with their logarithmic potential, i.e. $pK_A = -\log_{10}(K_A)$ and $pK_B = -\log_{10}(K_B)$. The surface charging condition, and thus φ_0 , at a certain pH can be solved with the known values of K_A and K_B , which, however, is a clumsy process with the classic site-binding model [52].

To overcome the complexity of the classic SBM, van Hal el. developed a general approach [53] to calculate the pH sensitivity. In their approach, the surface H^+ buffer capacity, $\beta_{\rm int}$, was introduced, to quantify the capability of an oxide surface to buffer the variation of the $H_{\rm S}^+$ concentration, so that a concise but physically meaningful expression for the pH sensitivity, S_{pH} , was found as follow:

$$S_{pH} = \frac{\Delta \varphi_0}{\Delta pH} = \frac{59.2 \text{ mV/}pH}{\frac{2.3kTC_{DL}}{q^2\beta_{int}} + 1}$$
(2.6)

where, q is the elementary charge. The calculation of β_{int} and C_{DL} depend on the charging mechanism and the EDL model to be applied, respectively. For the aforementioned SBM, β_{int} can be expressed as [53]:

$$\beta_{\text{int}} = \frac{1}{q} \frac{d\sigma_0}{dpH_S} = 2.3N_S \frac{D_2 K_B a_S}{D_1^2}$$
 (2.7)

where σ_0 denotes the surface charge density, $N_{\rm S}$ the density of surface OH group, and $D_{\rm I} = K_{\rm A}K_{\rm B} + K_{\rm B}a_{\rm S} + a_{\rm S}^2$ and $D_{\rm I} = K_{\rm A}K_{\rm B} + 4K_{\rm A}a_{\rm S} + a_{\rm S}^2$. On the other hand, $C_{\rm DL}$ can be calculated via the GCS model [50]. Hence, the $\varphi_0 - p{\rm H}$ relation, featured with $S_{p{\rm H}}$ in Eq (2.6), can be accurately determined, given that $\beta_{\rm int}$ and $C_{\rm DL}$ are evaluated via Eqs. (2.6) and (2.7). For the detailed calculation procedure the reader is referred to the cited literature. The signal of an ISFET, i.e. the change of $I_{\rm D}$ caused by that of $p{\rm H}$, can then be quantified, in accordance to the known transfer characteristic and $S_{p{\rm H}}$ of the ISFET.

2.2. Thermal noise in ion-sensing systems

2.2.1. Fluctuation-dissipation theorem

Thermal noise, also known as Johnson- Nyquist (J-N) noise, is caused by the random motion of charge carriers agitated thermally in an electrical conductor. It was detected by J. B. Johnson [54], and then was interpreted by H, Nyquist [55], with the thermally-agitated electromotive force in conductors. This noise is present in any substances that include charge carriers beyond T=0 K. Particularly in ion-sensing systems where liquid is involved, the electrons and holes in the solid electrodes and the ions in the liquid are all subjected to the thermal agitation, and thus generate the J-N noise. Its power spectral density (PSD) in terms of electrical potential is proportional to the real part of the electrical impedance spectrum Z(f) of the systems under test, which is expressed as [55]:

$$S_{V}(f) = 4kT \operatorname{Re}[Z(f)]$$
 (2.8)

where, f denotes frequency. Eq. (2.8) insightfully reveals the physical nature of the thermal noise of the charge carriers, generalized with the fluctuation-dissipation theorem [56]: the process in which the thermal agitation causes the random fluctuation of the carriers is equal to its reversed process where the kinetic energy of the moving carriers is transferred into heat through Re[Z(f)].

2.2.2. Electrochemical impedance spectroscopy

Eq. (2.8) is significant, not only because it provides fundamental understanding for the thermal noise, but the equation also points out that the thermal noise of a system can be probed by measuring its impedance spectrum. For ion-sensing systems in particular, the characterization of Z(f) refers to electrochemical impedance spectroscopy (EIS) [57], which usually employs a three-electrode measurement setup consisting of a working electrode

(WE), a counter electrode (CE) and a reference electrode (RE), as schematically shown in *Figure 6*. The WE is the electrode where electrochemical processes of interest are present; the CE is used to balance the current passing through the WE; the RE, with a known fixed electrode potential, acts as reference point for measuring and gauging the WE potential, ideally with no current flowing through it.

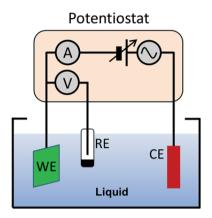


Figure 6. Three-electrode setup for EIS characterization. WE, RE and CE represent working, reference and counter electrode, respectively.

To perform an EIS measurement, a desired DC potential of the WE is firstly biased with respect to the RE, by applying a potential between the WE and CE. Then, an AC voltage at a certain frequency is applied on the WE with respect to the RE as well, and the responding AC current is recorded concurrently by an ammeter in the same current loop. Finally, Z(f) is obtained by dividing the AC voltage with the responding AC current at various sampling frequencies. All the controlling and measuring electronics, as well as data acquisition and analyzer, can be integrated as a compact instrument known as a potentiostat.

2.2.3. Constant phase element and 1/f noise

For purely resistive components such as metal leads, semiconductor and liquid bulk, Re[Z(f)] in Eq. (2.8) is reduced to a resistor, making S_v independent of f at a certain temperature, also known as white noise. However, more complicated impedance behaviors can appear locally, such as at solid/liquid interfaces, where Re[Z(f)] can be dependent on frequency and becomes significant under low frequencies.

The impedance for a charge-transferring Faradaic interface is expected to be a semicircle in a Nyquist diagram, centered on the x-axis, which can be represented by a simple equivalent circuit model consisting of a resistor R connected in parallel with a capacitor C [58]. However, the Nyquist plot of

the experimentally measured impedance data usually becomes a semicircle rotated around its high-frequency endpoint (left end), with its center lying below the x-axis [58]–[60], as illustrated in *Figure 7*(a). On the other hand, for blocking non-Faradaic systems such as insulating oxide/liquid interfaces, the electrochemical impedance in a Nyquist diagram often exhibits a straight line rotated around the high-frequency endpoint (lower end), with a phase angle smaller than 90°, instead of a vertical line represented by a pure C [59], as illustrated in *Figure 7*(b).

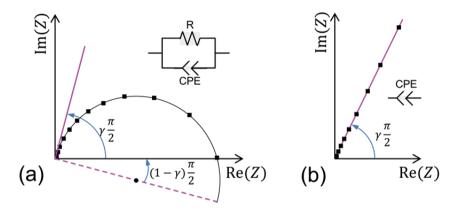


Figure 7. Typical impedance spectrum with CPE behaviors plotted in Nyquist diagrams for (a) Faradaic and (b) non-Faradaic systems, respectively.

These impedance behaviors cannot be accounted for by any simple R-C network, and are often represented by an phenomenological circuit component referred to as the constant phase element (CPE) [57], [61], with the impedance spectrum expressed as $Z_{\rm CPE}(f) = 1/Q(if)^{\gamma}$, where i is the imaginary unit, Q a CPE parameter and γ ranges from 0 to 1 in an electrochemical system [60]. Therefore, $S_{\rm V}$ of the thermal noise featured with the CPE behavior can be found as:

$$S_{\rm V}(f) = 4kT \, \text{Re}(Z_{\rm CPE}) = \frac{\cos(\pi \gamma/2)}{Q(2\pi)^{\gamma}} \frac{1}{f^{\gamma}}$$
 (2.9)

Note that $S_{\rm V}(f) \propto 1/f^{\gamma}$, and hence the J-N noise featured with the CPE behavior can be appreciably large as the frequency decreases. The noise with PSD subjected to this form is generally called 1/f noise. In the context of electrochemical systems, the physical interpretation of the CPE behavior is still under debate, although it is generally accepted [61], [62] either to root in spatial structural heterogeneities of electrodes [63]–[69] or to arise from varying time constants associated with different physical processes distributed at the electrode surface [70]–[76].

It should be noted that the 1/f noise appears in more than the liquid-involved systems. Some noise in the solid phases of the ion-sensing systems is also of the 1/f form, such as the channel fluctuation as discussed in Chapter 1. The latter, however, has been well addressed in the literature, and is beyond the scope of this thesis.

3. Enhance SNR via Internal Amplification

As discussed in Chapter 2, an ISFET system is inevitably faced with the interference from external noise. In terms of measurement practice, amplifying the internal signal without bringing in extra noise is an intuitive way to suppress the external interference, and thus improve SNR for the ISFET systems. This can be achieved by the new device concept demonstrated in this chapter. First, section 3.1 will discuss how the SNR is boosted via amplifying the internal signals, and then bipolar junction transistors (BJTs) will be introduced for the internal current amplification. The fabrication details of the designed amplifier will be described in section 3.2. Last, the DC performance of the fabricated device will be discussed in section 3.3, and noise performance benefiting from the device will be analyzed and discussed in section 3.4.

3.1. Internal signal amplification

Since signal current of an ISFET, ΔI_D , is relatively small, an external readout circuitry is commonly used to amplify the signal, as depicted in *Figure 8*.

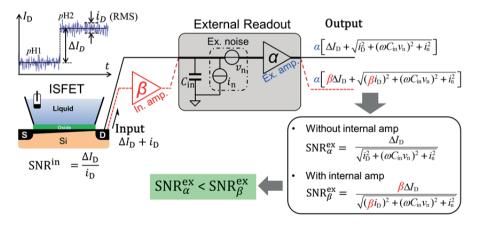


Figure 8. Schematic representation of an ISFET measurement system with an external readout. The red dashed line represents the signal flow with internal amplification. The external SNR with (SNR $_{\alpha}^{ex}$) and without (SNR $_{\beta}^{ex}$) internal amplification (β) are formulated, indicating SNR is boosted with the internal amplification.

Both $\Delta I_{\rm D}$ and the internal current noise $i_{\rm D}$ of the ISFET are amplified simultaneously. However, extra input current and voltage noise associated with the external readout circuitry, represented with $i_{\rm n}$ and $v_{\rm n}$ in *Figure 8*, is amplified and thus contributes to the total noise as well, making the external SNR (SNR $_{\alpha}^{\rm ex}$), as formulated in the figure, inferior to the internal one (SNR $^{\rm in}$).

In terms of the measurement practice, if the internal current of the ISFET, i.e. $\Delta I_{\rm D}+i_{\rm D}$, can be amplified before the external readout stage, without introducing extra noise, the external SNR will be altered to ${\rm SNR}_{\beta}^{\rm ex}$, as formulated in *Figure 8*. As long as β is large enough, the internal items, $\Delta I_{\rm D}$ and $i_{\rm D}$, in the ${\rm SNR}_{\beta}^{\rm ex}$ expression will dominate compared to the external noise, which leads to ${\rm SNR}_{\beta}^{\rm ex} > {\rm SNR}_{\alpha}^{\rm ex}$. This means the SNR in practice is improved by the internal amplification.

To avoid introducing additional noise, the internal amplifier should not introduce extra noise, and be placed as close to the output terminal of ISFET as possible. This can be achieved by a BJT which can be integrated with the ISFET tightly using standard CMOS technology. BJTs have two doping configurations, *pnp* and *npn*. Taking *pnp* type as an example, the BJT has two back-to-back PN junctions, forming three doped regions with different charge concentrations and polarities, as illustrated in *Figure 9*. The three regions of the BJT are *p*-doped emitter (**E**), *n*-doped base (**B**) and *p*-doped collector (**C**), respectively. The **E** region is heavily doped, while the doping levels of the other two are similar.

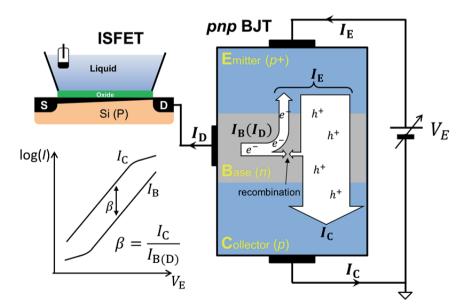


Figure 9. n-channel ISFET with drain connected to the base of a pnp BJT as the current amplifier. The typical log(I)- V_E plot of a BJT shows current amplification.

To operate the BJT, the **E-B** junction is forward biased, whereas the **B-C** junction is reverse biased, which can be performed by biasing a positive voltage between terminals **E** and **C**, as illustrated in *Figure 9*. Under the forward bias, many holes (h^+) in heavily doped **E** region are injected into lightly doped **B** region, whereas few electrons (e^-) diffuse back from **B** to **E**. On the other hand, minority of h^+ coming from the **E** region recombine with e^- in **B** region, while majority of them diffuse through the base and then be swept into the **C** region by the strong electric field between **B** and **C** caused by the reverse biased **B-C** junction. In terms of current through each terminal, the collector current I_C , almost identical to the emitter current I_E , is greater than the base current I_B , with a certain amplification ratio $\beta = I_C/I_B$, as illustrated in *Figure 9*.

3.2. Integration of internal current amplifier

The tight integration of the BJT to the ISFET was facilitated by designing a novel device, ion-gated bipolar amplifier (IGBA). The cross-sectional representation of the IGBA device is schematically shown in *Figure 10*. In the design, a laterally-diffused metal-oxide-semiconductor field-effect transistor (LDMOS-FET), acting as the modified ISFET, is laterally connected to the base of a vertical BJT. This way, the drain current, I_D , of the ISFET is immediately amplified by the BJT and leaves the device as a significantly enhanced collector current, I_C . As used in Ion Torrent technology and many other ion-sensing applications [77]–[80], an extended gate (EG) setup was employed for pH sensing demonstration. The EG structure in our setup is also schematically depicted in *Figure 10*, where, 1- μ m-thick aluminum is

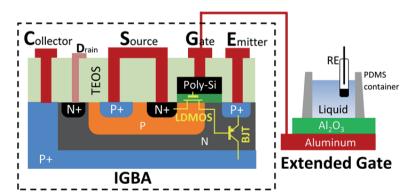


Figure 10. Schematic cross section of the IGBA device, as well as the EG-based pH measurement setup.

sputtered on a glass sheet, followed with the deposition of a 100-nm atomic-layer-deposited Al_2O_3 layer as the pH sensing material. A polydime-

thylsiloxane (PDMS) liquid container is glued on the EG, with a Ag/AgCl RE immersed in the solution to bias it.

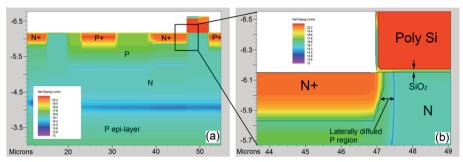


Figure 11. Simulated doping profile for (a) the whole IGBA device and (b) the zoom-in on the LDMOS-FET.

The IGBA device was fabricated via the standard silicon technology, and the simulated doping profile is shown in *Figure 11*(a). The substrate is a Borondoped $(5\times10^{18}~\rm cm^{-3})~p+(100)$ -bulk wafer with a 6.5-µm-thick Boron-doped $(1\times10^{15}~\rm cm^{-3})$ epitaxial layer. The p+ substrate serves as the C region of the BJT, being accessed with a p-ring plugged-in around the active area. The n region, formed by compensated Phosphorus implantation and thermal drivein, acts not only as the base of the vertical pnp BJT but also the drain of the n-channel LDMOS-FET. 25-nm-thick SiO₂, as labeled in *Figure 11*(b), was then grown by thermal oxidation, above which the poly-silicon gate stack was formed via low-pressure chemical vapor deposition (LPCVD) and reactive ion etching (RIE). The p-well was formed by B⁺ implantation, followed by a thermal annealing aiming not only to activate the dopants, but also to form a laterally diffused p-region under the gate stack as the n-

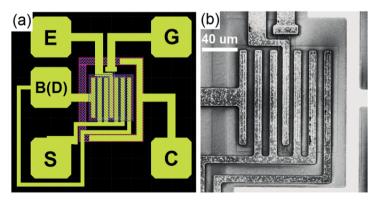


Figure 12. (a) Layout of contacting pads in photo lithography mask for the IGBA device. (b) Top-view of the central part of the fabricated device by SEM.

channel of the LDMOS-FET, as noted in *Figure 11*(b). The four heavily doped regions are the electrical accesses to the n-drain (\mathbf{D}), the p-substrate

and the n+ source (S) of the LDMOS FET, and the p+ E region of the BJT, respectively. 400-nm-thick tetraethyl orthosilicate (TEOS) was, then, coated as a preliminary passivation. Consequentially, other than terminals E and C of the BJT, the IGBA has another two terminals, source S and gate G, as depicted in the *Figure 10*. At the end of the fabrication flow, a layer of Aluminum was sputter-deposited, followed by RIE to form the contacting pads for all the terminals. The contacting pad layout of the designed device in the photo lithography mask is shown in *Figure 12*(a), and the top-view of the fabricated device via scanning electron microscopy (SEM) is shown in *Figure 12*(b).

3.3. DC Measurement of IGBA

The DC transfer characteristics, as well as the current amplification of the IGBA were characterized using an HP4155 precision semiconductor analyzer, as illustrated in *Figure 13*(a). During all the measurements, terminals **S** and **C** were biased at 0 V via two source measurement units (SMUs) of the HP4155 with respective to the common ground of the analyzer. For characterizing the transfer characteristics, the **E** terminal was biased with another

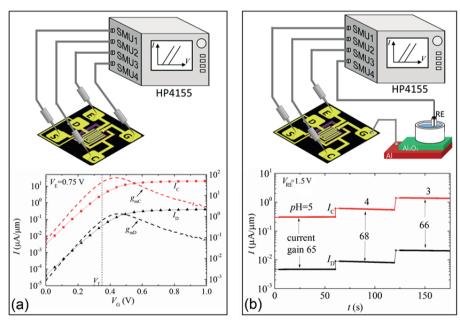


Figure 13. (a) $I_{\rm C}$ - $V_{\rm G}$ transfer and $g_{\rm mC}$ characteristics of the IGBA compared to $I_{\rm D}$ - $V_{\rm G}$ and $g_{\rm mD}$ of its reference ISFET and (b) $I_{\rm C}$ -t measurement for $p{\rm H}$ sensing with the IGBA compared to $I_{\rm D}$ -t of its reference ISFET, as well as the respective measurement setup. Note that $I_{\rm D}$ is equal to the measured $I_{\rm S}$.

SMU at a certain potential $V_{\rm E}$ =0.75 V above the built-in potential (about 0.6 V at room temperature) of the p+-n emitter-base junction to turn on the vertical BJT, and thus the whole device. Since $I_{\rm S}$ is almost equal to $I_{\rm D}$ of the ISFET, the measured value of $I_{\rm S}$ is regarded as $I_{\rm D}$ of the ISFET. $I_{\rm D}$ and $I_{\rm C}$ of the BJT were recorded simultaneously by the corresponding SMUs at varying $V_{\rm G}$, and they, as functions of $V_{\rm G}$, are depicted in Figure 13(a), in which the corresponding transconductances $g_{\rm mD}$ and $g_{\rm mC}$, defined as $g_{\rm mD}$ =d $I_{\rm C}$ /d $V_{\rm G}$ and $g_{\rm mC}$ =d $I_{\rm C}$ /d $V_{\rm G}$, are also shown. The threshold voltage, $V_{\rm T}$, is indicted in the figure with vertical broken lines. As seen, the current gain of the IGBA over the ISFET itself, i.e., $I_{\rm C}/I_{\rm D}$, is 60–80 in both weak inversion (subthreshold) (below $V_{\rm T}$) and moderate inversion (above $V_{\rm T}$) regions

For demonstrating pH measurement in electrolytes, the Al_2O_3/Al EG was bonded to terminal G, as illustration in Figure 13(b). The RE was then biased at a constant potential V_{RE} =1.5 V, and the variations of I_D and I_C with time, t, at different pH values in solution were monitored, as depicted in Figure 13(b). The pH values in the figure are nominal. They were altered manually by the titration of hydrogen chloride (HCl) into the solution. The results in the figure clearly demonstrate significant signal amplification of the IGBA in pH sensing applications

3.4. SNR Enhancement via IGBA

3.4.1. Characterization details

For the LFN characterization, the IGBA and its internal ISFET were analyzed separately. In both measurements, $V_{\rm G}$ was identical and so was $V_{\rm S}$ (grounded). $I_{\rm C}$ of the IGBA, as a function of time, was monitored at a certain $V_{\rm E}$ while $V_{\rm C}$ was grounded. The variation of $I_{\rm D}$ of the ISFET with the time was accessed via an additional contact to its drain terminal with a bias $V_{\rm D}$ (not shown in Fig. 1) while leaving terminals ${\bf C}$ and ${\bf E}$ unconnected. In order to make a fair comparison, $V_{\rm D}$ for the ISFET was set to render $I_{\rm D}$ identical to $I_{\rm S}$ of the IGBA. The biases in the terminals were applied using batteries. The fluctuation in $I_{\rm D}$ and $I_{\rm C}$ was first amplified by a TI TL071 lownoise preamplifier and then monitored at a sampling rate of 1000 Hz for 20 seconds using an Agilent B1530A Waveform Generator/Fast Measurement Unit. The current noise spectrum was analyzed using the signal processing toolbox in Matlab.

3.4.2. Results and discussion

The noise on I_D is inevitably amplified by the internal BJT. To quantify the noise and SNR, the PSD of the current noise as a function of f, was first characterized for I_C of the IGBA, denoted as S_I^{IGBA} , and I_D of the internal

ISFET, as $S_{\rm I}^{\rm ISFET}$. The $V_{\rm G}$ -referred PSD of voltage noise, $S_{\rm V}$, was then obtained by employing the following relationship:

$$S_{\rm V}^{\rm IGBA} = \frac{S_{\rm I}^{\rm IGBA}}{g_{\rm mD}^2}, \ S_{\rm V}^{\rm ISFET} = \frac{S_{\rm I}^{\rm ISFET}}{g_{\rm mC}^2}$$
(3.2)

The resultant $S_{\rm I}^{\rm IGBA}$ and $S_{\rm I}^{\rm ISFET}$ measured at $V_{\rm E}$ =0.75 V, with $V_{\rm G}$ biased at 0.25, 0.3 and 0.38 V are depicted in *Figure 14*(a), (b) and (c), which correspond to the subthreshold, weak inversion and strong inversion regimes, respectively. The dashed lines show the thermal noise of the ISFET under the same bias conditions for the corresponding case, calculated via $S_{\rm V}$ = $2/3 \times 4kT/g_{\rm mD}$. Two important observations can be found. First, the $S_{\rm I}^{\rm IGBA}$ curve is almost 10 times lower than the $S_{\rm I}^{\rm ISFET}$ ones in the entire measurement range from f=1 Hz to f=500 Hz. Second, the large spikes at 50 Hz and its higher harmonics in the ISFET are completely suppressed in the IGBA since they are smaller than the amplified signal.

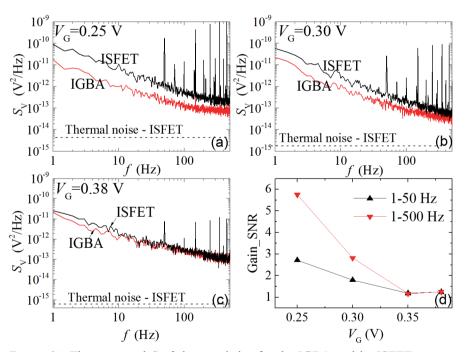


Figure 14. The measured $S_{\rm V}$ -f characteristics for the IGBA and its ISFET counterpart, at $V_{\rm E}$ =0.75 V and (a) $V_{\rm G}$ =0.25 V, (b) $V_{\rm G}$ =0.30 V and (c) $V_{\rm G}$ =0.38 V with the dashed line showing the corresponding calculated thermal noise of the ISFET under the same bias conditions. (d) Gain_SNR at different $V_{\rm G}$ for two frequency integration intervals in (a).

This much desired advantage with improved noise performance of the IGBA primarily results from signal amplification before it becomes contaminated by external interferences including noise generated by the low-noise preamplifier in the characterization system. As expected, the difference between $S_{\rm I}^{\rm IGBA}$ and $S_{\rm I}^{\rm ISFET}$ diminishes when $V_{\rm G}$ is increased above $V_{\rm T}$ at which both $I_{\rm C}$ and $I_{\rm D}$ increase by more than 100 times and the sensors themselves become noisier. Hence, the gain in SNR for the IGBA with referenced to the ISFET, which is calculated as:

$$Gain_SNR = \sqrt{\frac{g_{mC}^2}{\int S_1^{IGBA} df}} / \sqrt{\frac{g_{mD}^2}{\int S_1^{ISFET} df}} = \sqrt{\frac{\int S_V^{ISFET} df}{\int S_V^{IGBA} df}}$$
(3.3)

asymptotically approaches unity with increasing V_G , cf. Figure 14(b). The remaining SNR-benefit for the IGBA at $V_G \ge V_T$ is simply a consequence of the effective suppression of the spikes associated with 50 Hz and its harmonics. The effect of the spikes on Gain_SNR is better elucidated by including them in the SI integral from f=1 Hz to f=500 Hz; Gain_SNR is found to increase from 2-3 when the integration spans from f=1 Hz to f=50 Hz to around 6 when the integration range extends to f=500 Hz.

4. Assessment of Solid/Liquid Interface Noise in Ion-Sensing

In terms of the measurement practice, the noise performance for ion-sensing applications can be enhanced externally with the novel device concept, as detailed in Chapter 3. The internal SNR in ion sensing, however, cannot benefit from the same technology. On the other hand, reliable characterization tools for extracting the detailed information associated with the internal noise in ion sensing should always be the very first step on the way towards understanding the noise and even improving noise performance. Developing the tool will be the focus of the chapter. Section 4.1 will deal with the design and fabrication of the electrode cell dedicated for LFN characterization of an electrochemical system. Based on the electrode cell, related characterization techniques used will be detailed in section 4.2. At last, in section 4.3, the result of the noise measurement will be analyzed and discussed.

4.1. Differential microelectrode cell

4.1.1. Differential electrode configuration

As discussed in chapter 2, the noise characterization for the ISFETs is specialized on investigating the noise originating from the solid/liquid interfaces, which can be fulfilled with the differential electrode configuration, as will be introduced immediately.

Bearing native oxide that has a pH sensitivity close to the ideal Nernstian response with 59 mV/pH at room temperature [81], electrically conductive titanium nitride (TiN) was chosen as prototype sensing material of the electrode cell, in order to demostsrate its working principle. As schematically shown in *Figure 15*, the electrode cell was designed to have two identical TiN electrodes, in order to facilitate a direct assessment of the voltage noise via differential measurements. In the differential measurement, equal amount of DC potentials φ_{DL} across the EDL build up at the two identical $TiN|TiO_x|Iiquid$ intefaces, at a given pH value. As sensing surfaces are face-to-face in the measurement loop, their DC components (φ_{DL}) would cancel out with each other. In contrast, two identical AC voltage noise sources, denoted as v_n would be in series and independent of each other, as indicated in the schematics. Note that as long as the liquid concentration is high

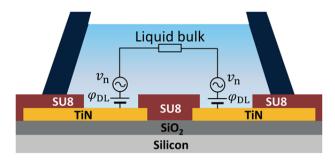


Figure 15. Schematic diagram of the differential microelectrode cell, in which φ_{DL} represents the DC potential across the EDLs, and v_n denotes the AC voltage noise sources.

enough so that the associated J-N noise is trivial, the total measured noise power would, then, be a summation of the contributions from the bulk electrolyte and the two EDLs.

4.1.2. Fabrication of the differential microelectrode cell

The microelectrode cell was fabricated via standard Si technology. First, a 100 nm thick TiN layer was sputtered on a Si wafer covered with a 500 nm thick thermally grown insulating SiO_2 layer. This was followed by photolithography in combination with reactive ion etching to define the microelectrode. Then, circular openings in SU8 2002 resist, with diameters 100, 300 and 1000 μm , were patterned using photolithography to expose the TiN surface to the sampling electrolyte, with the SU8 resist to passivate the rest of the cell. During noise measurement, the TiN electrodes were electrically bridged by the sampling electrolyte.

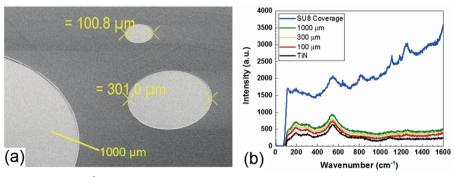


Figure 16. (a) 45°-tilt SEM images of the TiN sensing surface exposed after the SU8 passivation and patterning in the electrode cell. (b) Raman spectra of these exposed TiN sensing surface, as well as as-deposited TiN and the SU8 coverage.

The SU8 openings, inspected by SEM as presented in *Figure 16*(a), were confined within the patterned TiN area, thereby ensuring exposure of only the TiN surface to the electrolyte. The surfaces of the TiN electrodes were free from SU8 contamination within the detection limit of Raman spectroscopy, as shown in *Figure 16*(b).

4.2. Measurement methods

4.2.1 Potentiometric noise

The potentiometric measurement setup is schematically shown in *Figure 17*. The measurement loop comprises the two TiN electrodes and a KCl (Merck) aqueous solution as the sampling electrolyte, because KCl electrolyte is widely applied in (bio-) chemical sensing. The KCl concentration was varied from 1 mM to 1 M at two pH values 6 and 2. To measure the voltage noise, a preamplifier with a 0.1 Hz - 1 kHz bandpass filter and a gain of 10k was constructed using OPA140 operational amplifiers, and the signal was digitized using a Keysight U2351a multifunction data acquisition device. The electrical potential variation between the two electrodes was sampled at 10 kHz and 4 million data points were used to generate its voltage PSD, $S_{\rm V}^{\rm pot}$. The noise PSD was divided by 2 so as to normalize it to a single electrode.

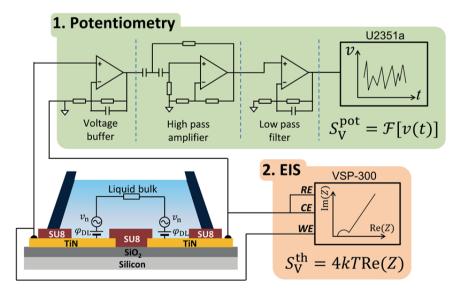


Figure 17. Schematic noise measurement setups for the TiN/KCl system with the differential microelectrode cell, via potentiometry specified in section 4.2.1 and EIS in section 4.2.2. It should be noted that the two measurement systems should work alternatively, which means only one of them is connected to the cell at a time.

4.2.2. Thermal noise

A comparison between the potentiometric and thermal noise give rise to insightful understandings of the interfacial noise. Thus, the thermal noise of the samples was characterized in the same solution as well. As discussed in Chapter 2, the thermal noise of liquid/solid systems can be probed via $S_{\rm V}^{\rm th} = 4kT{\rm Re}[Z(f)]$, in which Z(f) is the electrochemical impedance spectrum measured with a potentiostat via the three-electrode setup. For a differential configuration, however, the RE is no longer necessary, which is also a bonus of using the designed cell for EIS. As depicted in *Figure 17*, the EIS characterization with the designed cell was performed with a Bio-Logic VSP-300 potentiostat. The impedance spectrum was measured at 10 mV root-mean-square (RMS) AC from 100 mHz to 1 MHz. The measurement data was averaged over 30 cycles for each frequency point, and it was also divided by 2 to normalize it to a single electrode.

4.3. Result and discussion

4.3.1. $1/f^{\gamma}$ nature of oxide/electrolyte interfacial noise

Firstly, the measured $S_{\rm V}^{\rm pot}$ and $S_{\rm V}^{\rm th}$ of all the electrode areas are depicted together in *Figure 18*as the function of f for different TiN electrode areas. For the largest area in our design with a diameter of 1000 μ m, the lowest values of $S_{\rm V}^{\rm pot}$ are equal to the floor noise, $S_{\rm V}^{\rm floor}$ of the amplifier, for f > 50 Hz.

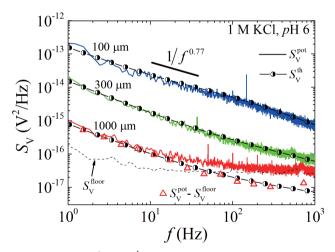


Figure 18. The measured $S_{\rm V}^{\rm pot}$ and $S_{\rm V}^{\rm imp}$ vs. f for all the three electrode areas. $S_{\rm V}^{\rm floor}$, depicted with the dashed-line, is the noise floor of the amplifier used in the potentiometric measurement.

As seen in the figure, for the smaller two sensing areas, an excellent agreement between S_V^{pot} and S_V^{th} in the entire measurement frequency range. For the biggest area, S_V^{pot} also matches with S_V^{th} to a great extent, by subtracting the influence of the noise floor. This verifies the absence of any major noise component other than J-N noise in the system [82].

In log-log scale, $S_{\rm V}^{\rm th}$ is observed to be linearly dependent on f with a slope – γ for all TiN electrode areas displayed. As discussed in Chapter 2, the low-frequency behavior of the electrochemical impedance can be described phenomenologically with the CPE [83], with $Z(f) = 1/Q(if)^{\gamma}$, and the frequency dependency of $S_{\rm V}^{\rm imp}$ on f follows a $1/f^{\gamma}$ relation, as featured with Eq. (2.9). Here, we obtain $\gamma = 0.77$ by linear fitting, as shown in *Figure 18*.

In a solid/liquid system, the thermal noise generated by liquid bulk should scale with electrode area A via a $1/\sqrt{A}$ dependence, because the bulk resistance, $R_{\rm b}$, can be approximated by its spreading resistance as $R_{\rm b} \propto K/\sqrt{A}$, with K as the resistivity of the liquid bulk [30]. On the other hand, the interfacial thermal noise should scale with 1/A, since the interfacial impedance is inversely proportional to A. Therefore, the contributions of the solid/liquid interface to the total thermal noise can be justified by investigating the dependence of the measured $S_{\rm V}^{\rm th}$ on A.

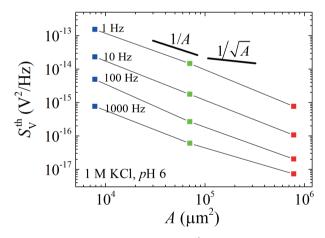


Figure 19. The dependence of the measured $S_{\rm V}^{\rm th}$ on A for all the electrode areas at different frequencies, where, the blue, green and red squares refer to 100, 300 and 1000 μ m openings, respectively. 1/A and $1/\sqrt{A}$ dependences are also depicted as reference.

In Figure 19, the dependence of the measured $S_{\rm V}^{\rm th}$ on A at varying frequencies for all the sample areas is depicted. As shown in the figure, $S_{\rm V}^{\rm th}$, except the largest area at the highest frequency, scales inversely with A and has a unity slope in the log-log scale for all the presented frequencies. This clearly indicates that the real part of the EDL impedance is much larger than $R_{\rm b}$, and

thus the interfacial thermal noise, with respect to that of the liquid bulk, prevails in the given experimental conditions.

Since $S_{\rm V}^{\rm pot}$ is in a great accordance with $S_{\rm V}^{\rm th}$ as illustrated in *Figure 18*, it can be inferred that the solid/liquid interfacial noise is subjected to the $1/f^{\gamma}$ form, showing its association with complex electrochemical processes at the interfaces.

4.3.2. Significant extrinsic noise in ISFETs

Finally, the area-normalized S_V of the 300 µm diameter TiN electrode is compared, in *Figure 20*, to the area-normalized input-referred noise of several state-of-the-art MOSFETs [84]–[86]. The comparison is made at 1 Hz and 10 Hz and includes different combinations of KCl concentration and pH value for the TiN electrode. It is apparent that the EDL noise is comparable or even higher than that of the reported advanced MOSFETs and cannot be neglected. Additionally, when the KCl concentration was reduced from 1 M to 1 mM at pH=6 with a negligible proton concentration, the observed change in S_V was too small to associate to an increase in R_b by about three orders of magnitude. This further confirms the minor role of the noise generated in the electrolyte bulk.

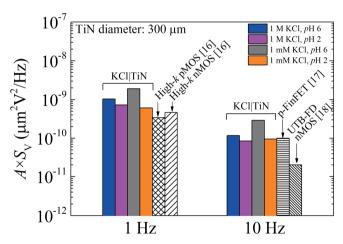


Figure 20. Comparison of area-normilized solid/liquid noise with the input-referred noise of several state-of-the-art MOSFETs at 1 and 10 Hz [84]–[86].

In contrast to the assumptions of others [30], [34], the real part of the measured sample impedance is much larger than the liquid impedance. We speculate that this is due to a rate limiting interfacial interaction or diffusion process at the liquid-solid boundary. It is striking, and has also been documented in the literature [82] that the voltage noise so closely follows the J-N formula. We believe that this is due to the fact that the presented oxide/liquid

system, measured under conditions of negligible current flow, is close to thermal equilibrium. Since the noise frequency dispersion is close to 1/f, it may be inferred that even 1/f noise obeys the J-N relation for systems close to thermal equilibrium. Another ubiquitous feature of these systems is the existence of the CPE with a phase between $-\pi/4$ and $-\pi/2$. No physical electrical network can give this relationship but it could be approximated by a non-uniform distributed network, which will be the topic of next chapter.

5. Electrochemical Impedance Modelling for Solid/Liquid Interface

In Chapter 4, it was concluded, from experimental viewpoint, that the LFN originating from the solid/liquid interface is of thermal nature, based on the excellent agreement between the potentiometric LFN and the real part of electrochemical impedance spectrum of the solid/liquid systems. Also, the interfacial noise was found to be subjected to a $1/f^{\gamma}$ form. In order to uncover the physics behind the $1/f^{\gamma}$ nature of the interfacial noise, in this chapter an impedance model is developed, based on the dynamic hydrogen ion binding reactions at oxide/electrolyte interface. Firstly, the modeling process will be presented in Section 5.1. The validity of the proposed model will then be justified in section 5.2, taking ALD TiO_2 films with different growth cycles as model samples.

5.1. Model development

5.1.1 Interfacial impedance based on site-binding reactions

Modelling the dynamics of a system is concerned with solving the corresponding dynamic equations. The dynamic rate equations for the H⁺ site-binding reactions (2.2a) and (2.2b) are given as

$$\frac{d[M-OH]}{dt} = c_{A}[M-O^{-}]a_{S} - r_{A}[M-OH], \qquad (5.1a)$$

$$\frac{d[M-OH_{2}^{+}]}{dt} = c_{B}[M-OH]a_{S} - r_{B}[M-OH_{2}^{+}]$$
 (5.1b)

In the context of impedance modeling, the solving process focuses on finding the dynamic current-voltage relations. For the oxide/electrolyte interface, the dynamic current arising from the dynamic processes described with Eqs. (5.1a) and (5.1b) are:

$$I_{A} = q \frac{\text{d[M-OH]}}{\text{d}t} = q N_{S} (c_{A} \Theta^{-} a_{S} - r_{A} \Theta^{0}),$$
 (5.2a)

$$I_{\rm B} = q \frac{d[\text{M-OH}_2^+]}{dt} = q N_{\rm S} (c_{\rm B} \Theta^0 a_{\rm S} - r_{\rm B} \Theta^+)$$
 (5.2b)

where, Θ^+ , Θ^- , and Θ^0 denote the fractions of protonated, deprotonated, and neutral OH groups, respectively. Θ^+ , Θ^- , and Θ^0 can be expressed as [53]:

$$\Theta^{+} = \frac{a_{\rm S}^{2}}{D_{\rm l}}, \quad \Theta^{-} = \frac{K_{\rm A}K_{\rm B}}{D_{\rm l}}, \quad \Theta^{0} = \frac{K_{\rm B}a_{\rm S}}{D_{\rm l}},$$
(5.3)

where, $a_{\rm S}$, $c_{\rm A}$, $c_{\rm B}$, and $D_{\rm 1}$ represent the same meanings respectively as in chapter 2. The solution of Eq. (5.2) is of the form of a two-branch admittance that naturally corresponds to the site-binding reaction, which can be solved by adding an AC voltage perturbation and making the small-signal approximation. The solving details can be found in Supporting Information (SI) of attached Paper III. The final expression for the site-binding admittance is:

$$Y_{SB} = \frac{sC_{buff} \left[1 + s \frac{1}{D_2} \left(\frac{a_S}{c_A} + \frac{K_A}{c_B} \right) \right]}{1 + \frac{s}{D_1} \left(\frac{a_S + K_B}{c_A} + \frac{a_S + K_A}{c_B} \right) + \frac{s^2}{D_1 c_A c_B}}$$
(5.4)

where, $s = j\omega$ with j as the imaginary unit and ω as angular frequency; C_{buff} is the capacitance associated with the buffer capacity β_{int} , calculated with:

$$C_{\text{buff}} = \frac{d\sigma_0}{d\varphi_S} = \beta_{\text{int}} \frac{dpH_S}{d\varphi_S} = \frac{q^2N_S}{kT} \frac{D_2K_Ba_S}{D_1^2}$$
 (5.5)

The EDL capacitance $C_{\rm DL}$ parallels with $Y_{\rm SB}$ network. Therefore, the total electrochemical impedance for the oxide/liquid interface, denoted as $Z_{\rm int}$, can be expressed as:

$$Z_{\rm int} = \frac{1}{sC_{\rm DL} + Y_{\rm SB}} \tag{5.6}$$

5.1.2 Variability in surface properties

It should be noted that a finite number of components appear in the circuit in *Figure 21*(a), which yields a semicircle centered on the x-axis in a Nyquist, and thus cannot interpret the CPE behaviors observed at the solid/liquid interfaces. A broad distribution of the surface properties needs to be taken into consideration in order to account for the CPE behavior, and it can be achieved by investigating possible mechanisms that would cause the varia-

tion of the kinetic parameters c_A and c_B , as well as thermodynamic parameters K_A and K_B .

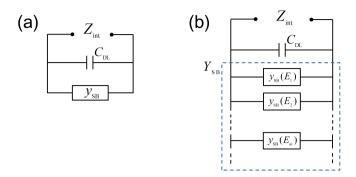


Figure 21. Equivalent circuits of the proposed oxide/liquid interfacial impedance model (a) without and (b) with energy distribution.

As specified in Chapter 2, $c_{\rm A}$, $c_{\rm B}$, $K_{\rm A}$, and $K_{\rm B}$ are by definition directly related to the energy states, i.e. the kinetic barriers, $E_{\rm A}^{\rm ad}$ and $E_{\rm B}^{\rm ad}$, and Gibbs free energies, $\Delta G_{\rm A}$ and $\Delta G_{\rm B}$, of the site-binding reactions. For an oxide surface evenly covered by discrete charged sites, H^+ adsorbed on/desorbed from the surface experiences an electrostatic force from the adjacent charged sites; therefore, those energies associated with the adsorption/desorption process are perturbed electrostatically [87], and thus are distributed over the surface. The detailed mechanism of the distribution can be complicated, but the stochastic nature of huge amounts of the binding sites can lead to a simplified treatment that the energies associated with the sites are assumed to comply with a normal distribution, and thus the site density per unit energy $N_{\rm SS}$ can be expressed as:

$$N_{\rm SS}(E_c) = \frac{N_{\rm S}}{\sigma_c \sqrt{2\pi}} \exp\left[-\frac{(E_c - E_{c0})^2}{2\sigma_c^2}\right],\tag{5.7a}$$

$$N_{\rm SS}(E_K) = \frac{N_{\rm S}}{\sigma_K \sqrt{2\pi}} \exp \left[-\frac{(E_K - E_{K0})^2}{2\sigma_K^2} \right]$$
 (5.7b)

where, the K subscript refers to the thermodynamic and the c subscript to the kinetic processes respectively. Therefore, K_A , K_B , c_A , and c_B , subjected to the exponential form shown in Eqs. (2.4) and (2.5), vary with the distributed energies, which are henceforward referred to as K-distribution and c-distribution, respectively, with the following expressions:

$$c_{A}(E_{c}) = c_{A0} \exp\left(-\frac{E_{c} - E_{c0}}{kT}\right), \quad c_{B}(E_{c}) = c_{B0} \exp\left(-\frac{E_{c} - E_{c0}}{kT}\right)$$
 (5.8a)

$$K_{A}(E_{K}) = K_{A0} \exp\left(-\frac{E_{K} - E_{K0}}{kT}\right), \quad K_{B}(E_{K}) = K_{B0} \exp\left(-\frac{E_{K} - E_{K0}}{kT}\right)$$
 (5.8b)

in which, the subscript 0 refers the variables to their respective values at E_0 . Note that the K-distribution implies a distribution in the thermodynamic equilibria of the reactions, whereas the c-distribution implies that in their kinetic barrier.

In general, these four distributions may be correlated to any degree or independent of each other. For simplicity in this treatment, the K-distributions, and likewise the c-distributions, are assumed to be completely correlated, while either the K or the c distributions will be investigated in turn, to see which matches the experimental data best.

Since Y_{SB} is a function of N_S , c_A , c_B , K_A , K_B represented with Eqs. (5.3), it is also dependent on the distributed energy, so that Z_{int} with the distributed energies should be expressed as:

$$Z_{\text{int}} = \frac{1}{sC_{\text{DL}} + \int y_{\text{SB}}(E) dE}$$
 (5.9)

where, y_{SB} denotes the density of Y_{SB} in the energy space. Eq. (5.9) is represented with the equivalent circuit in *Figure 21*(b), with y_{SB} represented as its discrete form.

5.2. Application of the proposed impedance model

5.2.1 Experimental procedure and parameter extraction

 TiO_2 has received much attention in pH-sensing applications [77], [79], [88], due to its superior chemical and physical stability. Thus, it was chosen as our sampling oxide. Concerning the electrode fabrication, a 100 nm thick Ti layer was first sputter-deposited on a glass wafer, which was followed by the deposition of a 40 nm thick TiN layer in the same sputtering system but in the presence of N_2 . This was followed by ALD of TiO_2 at 200 °C with $TiCl_4$ and H_2O as the reaction precursors. The deposition rate was estimated to be 0.045 nm per growth cycle by means of spectroscopic ellipsometry, yielding nominally a 1.8 nm thick TiO_2 fil with 40 cycles. The wafer was then diced into 10 mm \times 10 mm chips.

The schematic representation of the EIS measurement setup for the fabricated TiO₂ chips is depicted in *Figure 22*(a). In the setup, the TiO₂/TiN stack acts as the working electrode. The 0.2 M buffer solution (Merck Titrisol) was loaded in the reservoir glued on top of TiO₂, while an Ag/AgCl/3 M NaCl

RE and a Pt electrode as a counter electrode were submerged in the buffer. The pH value of the sampling buffer was 7.

The open circuit voltage (OCV) on TiN was firstly recorded using the Bio-Logic VSP-300 potentiostat. When the OCV readout became stable, the EIS measurement was performed. The impedance spectrum was measured at 10 mV RMS AC from 100 mHz to 1 MHz. The measurement data was averaged over 30 cycles for each frequency point.

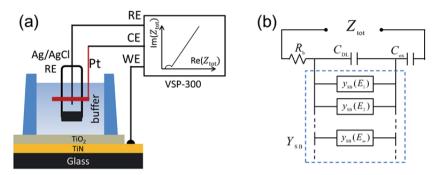


Figure 22. (a) Sketches of the electrode cell and the EIS measurement setup (b) Equivalent circuit of the buffer/TiO₂/TiN impedance Z_{tot} , with Y_{SB} in its discrete representation.

Note that both the liquid bulk resistance $R_{\rm b}$ and the TiO₂ capacitance $C_{\rm ox}$ are in series with $Z_{\rm int}$, as featured with the equivalent circuit in *Figure 22* (b). The parameters of the impedance model for $Z_{\rm int}$ proposed in section 5.1 can be extracted by numerically fitting the theoretical total impedance $Z_{\rm tot} = Z_{\rm int} + 1/sC_{\rm ox} + R_{\rm b}$ to the measurement data, with $C_{\rm ox}$ and $R_{\rm b}$ as modeling parameters as well. The details of the regression process can be found in SI of Paper III attached.

5.2.2. *K*-distribution vs *c*-distribution

As mentioned in section 5.1, the validities of K- and c- distributions should be justified by evaluating which one fits the experimental data best. Hence, the simulated $Z_{\rm int}$, with either distribution considered at a time, is compared with experiment for the 40 cycle ${\rm TiO_2}$ at $p{\rm H=7}$, as depicted in Figure 23. The optimized modeling parameters are summarized in Table 1, where, $p{\rm H_S} = -\log_{10}(a_{\rm S})$, as well as Θ_+ , Θ_0 , and Θ_- calculated via Eq. (5.3), are also listed.

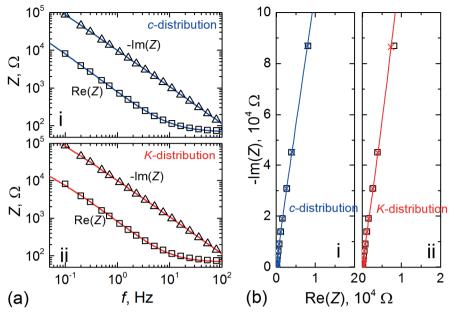


Figure 23. Comparison between simulation (curves and crosses) and measurement (squares and triangles) for the impedance with (i) the *c*-distribution and (ii) the *K*-distribution, depicted in (a) Bode plot and (b) Nyquist plot. Red symbols and curves refer to the *K*-distribution, while blue ones to the *c*-distribution. Black symbols refer to the measurement.

For the *K*-distribution, the simulation was also carried out with K_{A0} and K_{B0} as fitting parameters, depicted with red curves and crosses in plot ii) in *Figure 23*(a) and (b). Although the fitting is fairly good, it leads to a 100% negatively charged surface and negative pK values in Table 1, which is physically unreasonable. In addition, the obtained pH_S value at 13.4, as listed in Table 1, is unreasonably high, because it should be kept close to point of zero charge (PZC), around 6.2 for TiO_2 via $PZC = (pK_A + pK_B)/2$, owing to the large intrinsic buffer capacity of the oxide. All these results invalidate the *K*-distribution.

For the *c*-distribution, the simulation agrees well with the measurement. As the black curve in the Nyquist diagram shown in *Figure 23* (b) indicates, the proposed model accurately describes the CPE behavior of the TiO₂/electrolyte interface. The resulting surface charging is in a thermodynamic favorable condition where only a small fraction of the OH group is charged with the occupancy of -O⁻ site being slightly higher than that of -OH₂⁺, as shown in Table 1. The fitted $C_{\rm DL}$ value is comparable to our measured value of $C_{\rm DL}$ ranging from 0.2 to 0.3 Fm⁻² on a Pt electrode in the same solutions, as well as to the literature reported Stern capacitance $C_{\rm Stern}$ ranging from 0.2 to 1.4 Fm⁻² [53]. Moreover, the extracted binding site density $N_{\rm S} = 8.8 \times 10^{18}$ m⁻² is close to the reported range of 5-7×10¹⁸ m⁻² for TiO₂ anatase [89]–[91].

Table 1. Extracted modeling parameters for the K- and c-distributions for the 40 cycle TiO₂ in a pH=7 buffer. K_{A0} and K_{B0} refer to the values of K_A and K_B at the energy centroid, and likewise c_{A0} and c_{B0} to c_A and c_B .

		<i>K</i> -distribution	<i>c</i> -distribution
Modelling parameters	$R_{\rm b},\Omega$	68	68
	$C_{\rm ox}$, Fm ⁻²	0.34	0.52
	$C_{\rm DL}$, ${\rm Fm}^{-2}$	0.37	0.26
	$c_{\rm A},{\rm M}^{\text{-1}}{\rm s}^{\text{-2}}$	2.8×10^{10}	80.1
	$c_{\rm B},{\rm M}^{\text{-1}}{\rm s}^{\text{-2}}$	5.4×10^7	3.0×10 ⁻⁴
	pK_A	-3.2	7.7*
	pK_{B}	-4.2	4.7*
	a_{S}	4.2×10 ⁻⁸	0.57
	$N_{\rm S}$, $10^{-18} {\rm m}^{-2}$	7.3×10^6	9.0
	σ_K or σ_c , eV	0.18	0.18
Derived properties	pH _S	13.4	6.24
	Θ_{+}	0.0%	2.7%
	Θ_0	0.0%	94.0%
	Θ.	100.0%	3.3%

^{*} Specified as the reported values[89], [90]

The better agreement achieved with the c-distribution than the K-distribution indicates that the thermodynamic properties of the surface, represented by K_A and K_B , tend to be uniform over the surface, while the kinetic parameters would be strongly affected. This can be understood based on the notion that a conservative electrostatic potential can hardly change the Gibbs free energy of the binding reactions; the reaction kinetic barrier, however, can be readily affected by such electrostatic forces.

6. Understanding Oxide/Electrolyte Interface Noise

Based on the impedance model proposed in the last chapter, various surface properties of the solid/liquid interface can be extracted by comparing the theoretical impedance to the measurement data. The LFN originating from the interface, in turn, is linked to these surface properties. In this chapter, a comprehensive discussion will be made regarding how the noise is affected by the dynamic properties of the oxide/electrolyte interfaces. Except for the 40 cycle sample presented in the last chapter, two more samples with 20 and 60 cycle fabricated under the same conditions are added in the analysis, in order to introduce varying surface potteries. In Section 6.1 the noise modeling mothed will be analyzed. The results will then be presented and discussed in Section 6.2.

6.1. Noise modeling analysis

6.1.1. Parameter extraction

The main weakness of parameter extraction method for the proposed impedance model, as discussed in section 5.2.3, is the large number of parameters involved in the fitting procedure. In order to further constrain the modeling process, the values of $a_{\rm S}$, $N_{\rm S}$, and $C_{\rm DL}$ were solved by the classic SBM [53], with $S_{\rm pH}$ was measured for all the TiO₂ samples. The details can be found in SI of Paper IV appended. The oxide is believed not to contribute to the real part of the measured impedance, and then the noise of the TiO₂/buffer systems is attributed merely to the interfacial effect, and $C_{\rm ox}$ is on longer included for the noise analysis. Therefore, only $c_{\rm A0}$, $c_{\rm B0}$, and $\sigma_{\rm E}$ need to be determined numerically in terms of the noise analysis, and this can be achieved by numerically fitting the real part of $Z_{\rm int}$ in Eq. (5.8) to that of the measured TiO₂/buffer impedance. As mentioned at the beginning of this chapter, the 20 and 60 cycle samples fabricated in the same conditions are added in the analysis, in order to introduce varying surface potteries.

In Figure 24, the simulated interfacial noise $S_{\rm v}^{\rm n}$, calculated via $S_{\rm v}^{\rm n}(f) = 4kT \, {\rm Re}[Z_{\rm int}(f)]$, is depicted as a function of frequency, and compared with experimental (calculated from the real part of the measured

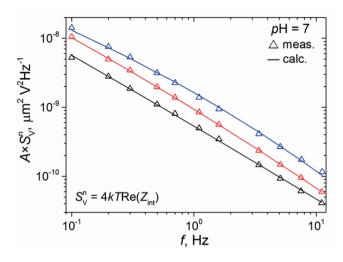


Figure 24. Comparison between simulated noise spectrum density depicted as solid lines and the experimental data calculated from real part of the measured impedance, depicted as triangels, for all the samples. Black, red and blue represent 20, 40, and 60 cycle samples, respectively

impedance via the same equation) for all the samples at pH 7, in which the bulk resistance R_b , extracted from high frequency data, has been subtracted. Note that excellent agreement is obtained in all cases. The values of all the modeling parameters are summarized in Table 2.

Table 2. Parameters for modeling the noise of the three processed samples at pH 7

Modelling para.	Note	20 cycle	40 cycle	60 cycle
S_{pH} , mV/ pH	Meas.	55.4	55	53.9
$N_{\rm S}10^{18}$	G1 : 6	10.0	9.0	7.0
$C_{\rm DL}$, Fm ⁻²	Calc. via S_{pH}	0.26	0.26	0.26
pK _A	Reported [89],	7.7	7.7	7.7
$p\mathrm{K}_\mathrm{B}$	[90]	4.7	4.7	4.7
$c_{A0}, M^{-1}m^{-2}$		7.8×10 ⁻³	78.8	7.5×10^{3}
$c_{\rm B0},{\rm M}^{\text{-1}}{\rm m}^{\text{-2}}$	Numerical fitting	1.3×10 ⁻¹⁴	2.4×10 ⁻⁴	1.6×10^{2}
σ_c , eV	nung	0.327	0.179	0.116

6.1.2. Noise dependence on the site-binding admittance

As discussed in Section 5.1, both the interfacial admittance $Y_{\rm SB}$ and $C_{\rm DL}$ contribute to $Z_{\rm int}$, and thus the interfacial noise. A static aspect, $C_{\rm DL}$, however, is not related to the surface dynamic properties. It is thus only $Y_{\rm SB}$ that reflects the contribution of the surface dynamics to the noise. For noise study, investigation of the real part of $Y_{\rm SB}$, compared to its imaginary part, is

more instructive because the interfacial noise, $S_{\rm V}^{\rm n}(f) = 4kT \operatorname{Re}[Z_{\rm int}(f)]$, is linked to $\operatorname{Re}(Y_{\rm SB})$ via the following expression:

$$Re(Z_{int}) = \frac{1}{|Y_{int}|^2} Re(Y_{int}) = \frac{1}{|Y_{int}|^2} Re(Y_{SB})$$
 (6.1)

Hence, $Re(Y_{SB})$, instead of the noise per se, acts as an indicator for investigating the noise dependence on the dynamic properties, which avoids clumsy consideration of C_{DL} . Specifically, the sample-dependent trend of $Re(Y_{SB})$ extracted from the measurement, as depicted in *Figure 25*(a), becomes the benchmark to which the trend of $Re(Y_{SB})$ calculated with the sample-dependent dynamic properties will be compared, as will be discussed momentarily.

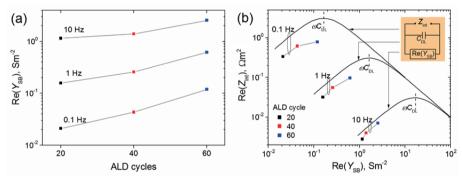


Figure 25. (a) Re(Y_{SB}) extracted from the EIS measurement at varying frequencies in order of the samples. (b) The dependance of Re(Z_{int}) on Re(Y_{SB}) extracted from the EIS measurement at varying frequencies for all the samples, in which the dependance of Re(Z_{int}) on Re(Y_{SB}) with Im(Y_{SB}) deliberately excluded is also depicted, shown as the solid curves.

The dependence of $Re(Z_{int})$ on $Re(Y_{SB})$ extracted from the EIS measurement, as represented with the colored squares in $Figure\ 25(b)$, can be analyzed semi-quantitatively by deliberately removing $Im(Y_{SB})$ from the Z_{in} network, which is featured with equivalent circuit in the figure. As the solid curves representing the circuit shown in $Figure\ 25(b)$, for all the presented frequencies, $Re(Z_{int})$ linearly increases with $Re(Y_{SB})$, as $Re(Y_{SB})$ is smaller than ωC_{DL} ; but the trend reverses from linearly increasing to decreasing, as $Re(Y_{SB})$ goes beyond ωC_{DL} . This predicted trend is followed well by the observed $Re(Z_{int})$ – $Re(Y_{SB})$ relation, as shown in the figure. Therefore, the dependence of the noise on $Re(Y_{SB})$ is determined by the relative size of the susceptance of C_{DL} to $Re(Y_{SB})$.

6.1.3. Averaging of distributed interfacial properties

As discussed in Section 5.1.2, the binding site density $N_{\rm S}$ per unit energy, i.e. $N_{\rm SS}$, is subjected to the normally distributed kinetic barrier E_c . Since the corresponding reaction rate constants $c_{\rm A}$ and $c_{\rm B}$ are exponentially dependent on E_c , it is expected that only a portion of the sites can respond to the external stimulation of EIS measurement, and thus contribute to the noise at a certain frequency, and so do the values of $c_{\rm A}$ and $c_{\rm B}$. One has to find out the representatives of these distributed properties for the whole surface, to order to facilitate the analysis of the noise dependence. This can be achieved by averaging their distributions with the distributed site-binding admittance $y_{\rm SB}(E_c)$ as a weighting factor. Choosing $y_{\rm SB}(E_c)$ as the weighting factor is based on the notion that the sites contribute to the noise by summing up $y_{\rm SB}(E_c)$ over the surface. Owing to the same reason discussed in the last subsection, ${\rm Re}[(y_{\rm SB}(E_c)]$ is used as the weighting factor.

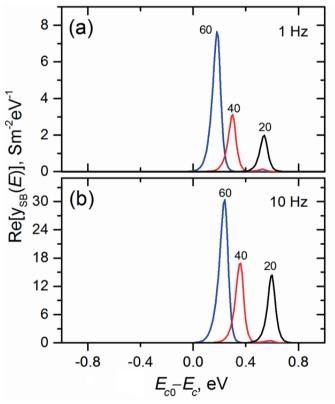


Figure 26. Re[$(y_{SB}(E_c)]$] dependent on the reaction barreir E_c , at (a) 1 Hz and (b) 10 Hz for all the samples.

In Figure 26, Re[$(y_{SB}(E_c))$] as a function of E_c is depicted at (a) 1 Hz and (b) 10 Hz, respectively. Only the sites $N_{SS}(E_c)$, and thus the corresponding

 $c_{\rm A}(E_c)$ and $c_{\rm B}(E_c)$, within the small ranges around the peaks of $y_{\rm SB}(E_c)$ contribute effectively. Their averages, i.e. $\langle N_{\rm SS} \rangle$, $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$, can then be calculated via:

$$\langle c_{\rm A} \rangle = c_{\rm A0} \exp \frac{\langle E_{c0} - E_c \rangle}{kT}, \quad \langle c_{\rm B} \rangle = c_{\rm B0} \exp \frac{\langle E_{c0} - E_c \rangle}{kT}$$
 (6.2a)

$$\langle N_{\rm SS} \rangle = \frac{N_{\rm S}}{\sigma_c \sqrt{2\pi}} \exp{-\frac{\langle E_{c0} - E_c \rangle^2}{2\sigma_c^2}}$$
 (6.2b)

where $\langle E_{c0} - E_c \rangle$ is calculated with:

$$\langle E_{c0} - E_c \rangle = \frac{\int (E_{c0} - E_c) \operatorname{Re}[y_{SB}(E_c)] dE}{\int \operatorname{Re}[y_{SB}(E_c)] dE}$$
(6.3)

The average of $y_{SB}(E)$, i.e. $\langle y_{SB} \rangle$, can then be represented as well by substituting $N_{SS}(E)$, $c_A(E)$ and $c_B(E)$ in Eq. (5.4) with their average values.

6.2. Correlation of LFN to surface dynamic properties

6.2.1. Effect of reaction rate constant

In Figure 27(a), $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$, calculated with Eq. (6.2a), are depicted in order of ALD samples at three different frequencies, 0.1, 1, and 10 Hz. As seen, both $\langle c_A \rangle$ and $\langle c_B \rangle$ are dependent on f; at a given f, $\langle c_A \rangle$ is almost identical for all samples independent of the number of deposition cycles, but $\langle c_{\rm B} \rangle$ increases by 10 orders of magnitude as the ALD process increases from 20 to 60 cycles. To elucidate this, the schematic frequency response of the real part of a single branch y_{SB} is plotted in Figure 27(b), where Re(Y_{SB}) , as the envelope of several y_{SB} branches, is also plotted. It is seen that each branch contributes to $Re(Y_{SB})$ mainly near its corner frequency f_c , which corresponds to the admittance contribution within a narrow E_c range at a certain frequency, as shown in Figure 26. Therefore, at a given measurement frequency $f_{\rm M}$, only the branches that have $f_{\rm c}$ close to $f_{\rm M}$ will contribute to $Re(Y_{SB})$. The relationship between f_c and the surface properties was found to be proportional to $c_A(E_c)$ for any branch (see SI of Paper IV). Thus, at a specified $f_{\rm M}$, $\langle c_{\rm A} \rangle$ should be proportional to $f_{\rm M}$, estimated as (see SI of Paper IV):

$$\langle c_{\rm A} \rangle = \frac{2\pi}{a_{\rm S}} f_{\rm M} \tag{6.4}$$

Since a_S is kept constant by a large C_{buff} for similar surfaces at the same pH, $\langle c_{\rm A} \rangle$ will be determined mainly by $f_{\rm M}$ and is not expected to vary much from sample to sample. Eq. (6.4) also clearly indicates that at low $f_{\rm M}$, the sites with low $\langle c_A \rangle$ (high kinetic barrier E_c) contribute dominantly to Re(Y_{SB}) and thus LFN, while those with high $\langle c_A \rangle$ (low E_c) contribute only at higher $f_{\rm M}$. However, since $Y_{\rm SB}$ is in parallel with $C_{\rm DL}$, the contribution from the sites with low E_c to the noise will be shorted by C_{DL} at high frequencies. Since f_c is observed to be independent of $c_{\rm B}$, it becomes apparent that the -O sites, rather than the neutral -OH sites, determine the surface dynamics and thus the noise, as a result of the much larger reaction rate of the -O sites than that of the -OH sites. By substituting $\langle c_A \rangle$ and $\langle c_B \rangle$ for each samples in Eq. (5.4), $q^2 N_{\rm SS}(E)/kT$ -normalized Re[$\langle v_{\rm SB} \rangle$] is depicted in Figure 27(c) at the three frequencies. As seen, the increment of the normalized Re[$\langle y_{SB} \rangle$] at a given frequency is less than a factor of 2 from 20 to 60 growth cycles, which is the direct result of the invariability of $\langle c_A \rangle$ and thus distinctly differs from the observed trend of $Re(Y_{SB})$ in Figure 25(a).

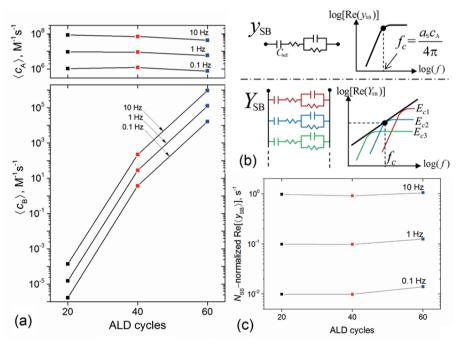


Figure 27. (a) Sample-dependent $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$ at varying frequencies. (b) Schematic frequency responses of Re($y_{\rm SB}$) and Re($Y_{\rm SB}$). Details of the equivalent circuit of the single branch can be found in Paper III. (c) $N_{\rm SS}$ -normalized Re[$\langle y_{\rm SB} \rangle$] in order of the samples at the three different frequencies.s

6.2.2. Effect of site density

As for the contribution of $N_{\rm SS}$ to the interfacial LFN, similar to $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$, $\langle N_{\rm SS} \rangle$ was first calculated via Eq. (6.2b) and then depicted in order of samples at varying frequencies in *Figure 28*(a). As depicted in the figure, $\langle N_{\rm SS} \rangle$ increases from 20 to 60 cycles sample at a certain f. Using $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$, Re[$\langle y_{\rm SB} \rangle$] was calculated and depicted in order of samples at the three frequencies in *Figure 28*(b). Re[$\langle y_{\rm SB} \rangle$] resembles well the observed sample-dependent variation of Re($Y_{\rm SB}$) in *Figure 25*(a). Since the variations of $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$ hardly interpret the trend of Re($Y_{\rm SB}$), the variation of $\langle N_{\rm SS} \rangle$ should account for it, and thus for the LFN.

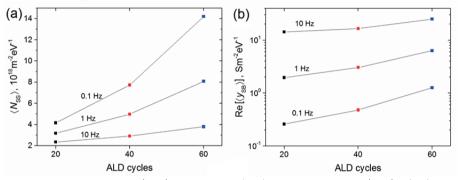


Figure 28. Figure 6. (a) $\langle N_{\rm SS} \rangle$ and (b) $\text{Re}(\langle y_{\rm SB} \rangle)$ calculated with $\langle N_{\rm SS} \rangle$, $\langle c_{\rm A} \rangle$ and $\langle c_{\rm B} \rangle$ at varying frequencies in (b).

6.2.3. Summarized remarks

As shown in *Figure 29* with three site-binding branches characterized by E_{c1} to E_{c3} for illustration, the noise spectrum envelope consists of contributions from distributed site-binding branches with different kinetic barriers E_c . It is the sites with large E_c that would contribute most to the noise in the low-frequency regime; the amplitude of the LFN is primarily determined by N_{ss} with large E_c . Therefore, to minimize the LFN, reducing the N_{ss} with large E_c can be an effective approach.

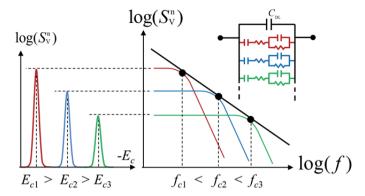


Figure 29. Schematic dependence of LFN on E_c , as well as and its frequency spectrum. The three colored lines illustrate contributions from three site-binding reaction branches with different kinetic energy barriers, E_{c1} , E_{c2} , and E_{c3} .

7. Concluding Remarks and Future Perspective

In summary, this thesis peruses an insightful understanding of the LFN arising in ion sensing devices, with ISFETs as a particular focus. For this purpose, the research work starts firstly with the discussion of the proposed semiconductor device for an enhanced SNR for the ISFETs. Then, the fabrication and characterization of the differential microelectrode array archives the accurate measurement of solid/liquid interfacial noise. At the end, electrochemical impedance model is developed based on the interfacial properties for interpreting the interfacial noise, which is immediately followed by a thorough discussion about the dependence of the noise on the surface dynamic properties. Upon the extensive work, the major achievements are summarized as follows:

- 1. Motivated with the internal amplification to diminish the external interference, the IGBA device was designed and fabricated, which is featured with the intimate integration of an ISFET with a low-noise vertical BJT. The internal amplification was achieved by the immediate and direct current amplification of the BJT, yielding a 70-fold internal current gain, and the IGBA's efficacy of enhancing SNR was clearly demonstrated by comparing its noise performance to that of the ISFET alone. The high current gain also applies when the device is used for pH sensing. These characteristics make the IGBA competitive in applications such as genome sequencing which are prone to be affected by the external interference owing to a dense integration of ion sensors.
- 2. The differential microelectrode array was fabricated, and the solid/liquid interfacial noise was accurately assessed based on the fabricated cell. The characterization incorporated both potentiometry and EIS concurrently for the noise measurement. The measured poteiometric noise is found to coincide quantitatively with the thermal noise calculated from the measured impedance, evidencing the noise originating from the TiN/electrolyte interface is of thermal nature.
- 3. The solid/liquid interface noise is found to be comparable or even larger than the input-referred noise of the state-of-the-art MOSFETs. Therefore, its influence cannot be overlooked for design of future ion sensors
- 4. Based on the SBM describing the H⁺ reactivity at the oxide/liquid interfaces, a dedicated electrochemical impedance model was derived. The model not only incorporates both thermodynamic and kinetic properties of the site-binding reactions, but further takes into consideration the distributed nature

of the characteristic energy of the binding sites, so as to account for the interfacial impedance featured with the CPE behavior. With the model, the solid/liquid interfacial LFN is clearly linked to the thermodynamic and kinetic properties of the oxide surface.

- 5. The derived impedance model was used to investigate the correlation of the LFN to the averaged reaction rate constants and binding site density. c_A is found to be determined mainly by the measurement frequency f_M . At a given f_M , it will not vary too much among samples, and thus cannot account for the corresponding noise variation.
- 6. The noise spectrum consists of contributions from distributed sitebinding branches with different kinetic barriers E_c . It is the sites with large E_c that would contribute dominantly to the noise in the low-frequency regime; the amplitude of the LFN is primarily determined by N_{ss} with large E_c .

Through this work, the extensive knowledge regarding the origination and mechanism of the noise of solid/liquid systems has been gained, being a dispensable step towards even more insightful understanding of the solid/liquid systems. To this end, extra efforts can be placed as follows:

- 1. The extended-gate configuration can be integrated tightly with the IG-BA devices in the same chip, in order to minimize any possible coupling of external interference. On the other hand, the integration of the two components as a robust *pH* measurement platform has vast potential to benefit the corresponding sensing applications.
- 2. The over-simplified model for super thin oxide layers would limit application of the proposed interfacial impedance model. A more accurate model can be applied to the oxide, which should be assisted with more detailed characterizations on the oxide surface morphology, thickness and dielectric properties etc.
- 3. It is intereting to explore other mechanisms behind the distributed energy proposed in the model than the static charging on the surface. In particular, the physical meaning of σ_c can be explored.
- 4. It is interesting to explore the dependence of the solid/liquid interfacial noise on the interfacial thermodynamic properties, i.e. K_A and K_B , which can be performed by investigating the solid/liquid noise of varying oxides.

Summary of the Appended Papers

Paper I presents an ion-gated bipolar amplifier (IGBA) featured with internal current amplification. The IGBA device, fabricated with standard CMOS technology, consist of an ISFET tightly integrated with a low-noise vertical BJT for internally amplifying signal current from the ISFET up to 70-fold. The internal amplification significantly suppresses the interference from external noise, which leads to an SNR improvement compared to its ISFET reference. The high current gain also applies when the device is used for pH sensing. Applications like genome sequencing are susceptible to the external interference due to a dense integration of huge amount of sensors. Thus, the efficacy of suppressing external interference makes the IGBA-based sensors suitable for these applications.

Paper II presents the fabrication and characterization of a microelectrode cell dedicated for assessment of the solid/liquid interface noise without recourse to a reference electrode. In the electrode cell, two identical TiN electrodes of various sizes are designed for differential measurements. Both potentiometry and EIS were applied to the fabricated electrode cell for the assessing the interfacial noise. The measured poteiometric noise almost equals to the thermal noise calculated from the measured impedance, indicating the noise from the TiN/electrolyte system is of thermal nature. Scaling inversely with electrode area, the noise is concluded to mainly arise from the solid—liquid interface. Besides, the solid/liquid interface noise is found to be comparable or even larger than the input-referred noise of the state-of-the-art MOSFETs. Therefore, its influence cannot be overlooked for design of future ion sensors

In **Paper III**, a dedicated electrochemical impedance model is developed, based on the H⁺ reactivity at the oxide/liquid interfaces described by the SBM. The model is derived from the dynamic rate equations of the amphoteric H⁺ site-binding reactions, incorporating both thermodynamic and kinetic properties of the reactions. By taking into account the distributed nature of the kinetic barriers of the binding sites, the model is found to give an excellent agreement with the measured impedance including attaining reasonable modeling parameters, which confirms that the CPE behavior of the solid/liquid interface can be accounted for by the variability of the kinetic barriers of the H⁺ site-binding reactions. With the model, the solid/liquid interfacial LFN is linked to the thermodynamic and kinetic properties of the oxide surface.

Paper IV investigates the dependence of the noise on the averaged reaction rate constants and binding site density by using the impedance model developed in **Paper III**. The study unveils that the variation of interfacial noise is primarily caused by that of averaged binding site density, rather than the reaction rate constants. The sites with large kinetic barriers E_c that would contribute dominantly to the noise in the low-frequency regime; the amplitude of the LFN is primarily determined by $N_{\rm ss}$ with large E_c . Therefore, to minimize the LFN, reducing the $N_{\rm ss}$ with large E_c can be an effective approach.

Sammanfattning på svenska

Den enorma vetenskaplig och kommersiell betydelse som finns av att dechiffrera den mänskliga genetiska koden har startat en revolution inom genom-sekvenseringstekniken. Den första fullständiga sekvenseringen av människans genom uppnåddes genom det humana genomprojekt (HGP) 2003, då genom att använda den traditionella Sanger-metoden. Under årtiondena efter HGP hade slutförts kom en uppsjö av tekniska innovationer ut till forskningsgemenskapen och sekvenseringsmarknaden. Alla dessa innovativa sekvenseringstekniker har bidragit till betydligt kortare testtider och till lägre kostnader jämfört med de traditionella metoderna, detta tyder på en framtid med prisvärd personlig diagnostik och behandling.

Jon Torrent-sekvenseringstekniken, en av de nyaste sekvenseringsmetoderna, har haft en stor påverkan på sekvenseringsfältet. Detta på grund av dess förmåga att integrera ytplacerade sensorer med avläsningskretsar på baksidan, tillverkade med CMOS-tekniken. Sekvenseringsprincipen för Jon Torrent-metoden är enkel. Det enkelsträngade DNA:t utsätts sekventiellt för de fyra typerna av deoxinukleosidtrifosfat (dNTP), A, C, G eller T. När en inkommande dNTP är komplementär till nästa icke-parade nukleotid på DNA kedjan reagerar dom och frigör en proton (H⁺) som sedan kan detekteras av proton -sensorer.

De protonsensorerna som används i Jon Torrent-sekvensering är jonkänsliga fälteffekttransistorer (ISFET). En ISFET är en halvledarkomponent som kan tillverkas med standard CMOS-teknik. Vanligtvis tillverkas dessa av ett måttligt dopat kiselsubstrat med två kraftigt dopade områden i motsatt polaritet till substratet, dessa verkar som source och drain. Mellan source och drain går det en ledande kanal med ett lager av oxid ovanpå. Under en mätning sätts oxidytan i kontakt med en vätska och när vätskans pH varierar för att bibehålla ytjämvikten kan de amfotära hydroxyl (OH) -grupperna på oxidytan fånga/släppa protonerna. Som följd av denna mekanism uppstår det en variation i ytladdningen. Sålunda kommer oxidens elektriska potential φ_0 att förändras och den förändringen kommer att påverka kanalen under oxiden, vilket orsakar en ändring i kanalens genomsläppta ström (I_D). Förståelse för operationsprincipen hos en ISFET är beroende av hur φ_0 varierar med pH:t. Detta har väl beskrivits genom platsbindningsmodellen (SBM) som beskriver hur proton-reaktiviteten vid oxid/vätskegränsskiktet korrekt kan kvantifieras.

Däremot är det inte så att integreringen av flera sensorer alltid är till någon fördel. Försämringen av brusprestandan för ISFET-enheterna och allvarliga internkontamineringar mellan de integrerade kretsarna kan markant påverka sekvenseringsnoggrannheten. För Jon Torrent-sekvenseringen betyder en enkelbaskoppling till DNA:t en förändring av 0,02 i pH:t, detta motsvarar omkring 1 mV-förändring i φ_0 enligt Nernst-ekvationen. För att mäta en sådan liten potentiell förändring så måste bruset i sensorn sänkas till en acceptabel nivå. Den största delen av bruset i jonavkännande komponenter kan ses i lågfrekvensregimen, det är också där sensorexperimenten typiskt utförs. Dessutom så kan en hög densitet av metall delar i sensorchipset resultera i lågfrekventa interferenser som kan störa de biomedicinska signalerna som finns i samma frekvensdomän. Därför blir lågfrekvent brus (LFN) en av de viktigaste prestanda parametrarna för jonkänsliga FET-system

För ett ISFET-baserat sensorsystem kan bruset ha sitt ursprung utanför sensor, från t.ex. omgivningen och mätinstrumenten. Dessa yttre källor kan försummas genom att internt förstärka ISFET:s signaler, vilket förbättrar det mätta signal-brusförhållandet (SNR). Med den motiveringen av behovet av intern signalförstärkning designade och tillverkades nya jonavsensorer, dvs jonkontrollerad bipolär förstärkare (IGBA). IGBA-enheten är utrustad med en nära integration med en ISFET och en brusdämpande vertikal bipolär förbindelsestransistor (BJT). Den interna förstärkningen uppnåddes genom omedelbar och direkt koppling till BJT:n, vilket gav en 70-faldig internströmförstärkning. IGBA: s effektivitet för förbättring av SNR visades tydligt genom att jämföra dess brusprestanda mot den av en ensam ISFET. Högströmförstärkningen gäller också när enheten används för pH-mätningar. Dessa egenskaper gör den IGBA-baserade jonsensorn särskilt attraktiv inom områden som genom-sekvensering vilket kräver storskaliga, tättintegrerade jon-sensorer som kan snabbt generera en stor mängd data.

Brus inuti en ISFET kallas för ISFET:s interna brus. För de olika interna bruskällorna saknas det en systematisk studie för det fasta/flytande gränssnittet. För att exakt kunna bedöma gränssnittet i en LFN tillverkades en specifik differential-mikroelektrodmatris användes för som att karakterisera TiN/elektrolytgränssnittet. Karakteriseringen av bruset bestod av både potentiometri och elektrokemisk impedansspektroskopi. Det uppmätta potentiometriska bruset visade sig sammanfalla kvantitativt med det termiska bruset beräknat från den reella delen av den uppmätta impedansen. Detta visar att LFN som kommer från TiN/elektrolytgränssnittet är av termisk natur. Dessutom så är gränssnittsbruset jämförbart och till och med större än det mätta bruset från toppmoderna MOSFET:s. Denna felkälla kan därför inte förbises för design av framtida jon-sensorer

Bortsett från experimentella resultat ger den här avhandlingen en inblick i förståelsen av LFN som kommer från den jon interaktionen vid det fasta/flytande gränssnittet. För att klargöra detta presenteras här en elektrokemisk impedansmodell baserad på de gränssnittsegenskaperna som kan

resultera i gränssnittets LFN. Modellen innefattar inte bara de termodynamiska och kinetiska egenskaperna hos de adsorberande reaktionerna utan tar även hänsyn till den karakteristiska naturen hos bindningssätena. Detta tillåter modellen att hantera gränssnittsimpedansen som presenteras med det konstanta faselementets beteende. Med modellen är det fasta/flytande gränssnittens beteende uppenbart kopplat till de termodynamiska och kinetiska egenskaperna hos oxidytan.

Den härledda impedansmodellen användes för att undersöka om bruset var beroendet av de genomsnittliga reaktionshastighetskonstanterna och bindningsstätheten. Det visade sig att variationen av gränssnittsstörningar huvudsakligen orsakades av den genomsnittliga bindningsställdensitet snarare än reaktionshastighetskonstanterna

Genom detta arbete har den omfattande kunskapen om brusets uppkomst och mekanism utvecklats, vilket är ett viktigt steg mot ännu mer insikt och förståelse av fasta/flytande gränsskikt.

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Reference

- [1] B. J. West and M. Shlesinger, "The Noise in Natural Phenomena," *Am. Sci.*, vol. 78, no. 1, pp. 40–45, 1990.
- [2] J. C. Venter, M. D. Adams, E. W. Myers, P. W. Li, R. J. Mural, G. G. Sutton, H. O. Smith, M. Yandell, C. A. Evans, R. A. Holt, J. D. Gocayne, P. Amanatides, R. M. Ballew, D. H. Huson, J. R. Wortman, Q. Zhang, C. D. Kodira, X. H. Zheng, L. Chen, M. Skupski, G. Subramanian, P. D. Thomas, J. Zhang, G. L. Gabor Miklos, C. Nelson, S. Broder, A. G. Clark, J. Nadeau, V. A. McKusick, N. Zinder, A. J. Levine, R. J. Roberts, M. Simon, C. Slayman, M. Hunkapiller, R. Bolanos, A. Delcher, I. Dew, D. Fasulo, M. Flanigan, L. Florea, A. Halpern, S. Hannenhalli, S. Kravitz, S. Levy, C. Mobarry, K. Reinert, K. Remington, J. Abu-Threideh, E. Beasley, K. Biddick. Brandon, Bonazzi, R. M. Chandramouliswaran, R. Charlab, K. Chaturvedi, Z. Deng, V. Di Francesco, P. Dunn, K. Eilbeck, C. Evangelista, A. E. Gabrielian, W. Gan, W. Ge, F. Gong, Z. Gu, P. Guan, T. J. Heiman, M. E. Higgins, R.-R. Ji, Z. Ke, K. A. Ketchum, Z. Lai, Y. Lei, Z. Li, J. Li, Y. Liang, X. Lin, F. Lu, G. V Merkulov, N. Milshina, H. M. Moore, A. K. Naik, V. A. Narayan, B. Neelam, D. Nusskern, D. B. Rusch, S. Salzberg, W. Shao, B. Shue, J. Sun, Z. Y. Wang, A. Wang, X. Wang, J. Wang, M.-H. Wei, R. Wides, C. Xiao, C. Yan, A. Yao, J. Ye, M. Zhan, W. Zhang, H. Zhang, Q. Zhao, L. Zheng, F. Zhong, W. Zhong, S. C. Zhu, S. Zhao, D. Gilbert, S. Baumhueter, G. Spier, C. Carter, A. Cravchik, T. Woodage, F. Ali, H. An, A. Awe, D. Baldwin, H. Baden, M. Barnstead, I. Barrow, K. Beeson, D. Busam, A. Carver, A. Center, M. L. Cheng, L. Curry, S. Danaher, L. Davenport, R. Desilets, S. Dietz, K. Dodson, L. Doup, S. Ferriera, N. Garg, A. Gluecksmann, B. Hart, J. Haynes, C. Haynes, C. Heiner, S. Hladun, D. Hostin, J. Houck, T. Howland, C. Ibegwam, J. Johnson, F. Kalush, L. Kline, S. Koduru, A. Love, F. Mann, D. May, S. McCawley, T. McIntosh, I. McMullen, M. Moy, L. Moy, B. Murphy, K. Nelson, C. Pfannkoch, E. Pratts, V. Puri, H. Qureshi, M. Reardon, R. Rodriguez, Y.-H. Rogers, D. Romblad, B. Ruhfel, R. Scott, C. Sitter, M. Smallwood, E. Stewart, R. Strong, E. Suh, R. Thomas, N. N. Tint, S. Tse, C. Vech, G. Wang, J. Wetter, S. Williams, M. Williams, S. Windsor, E. Winn-Deen, K. Wolfe, J. Zaveri, K. Zaveri, J. F. Abril, R. Guigó, M. J. Campbell, K. V Sjolander, B. Karlak, A. Kejariwal, H. Mi, B. Lazareva, T. Hatton, A. Narechania, K. Diemer, A. Muruganujan, N. Guo, S. Sato, V. Bafna, S. Istrail, R. Lippert, R.

- Schwartz, B. Walenz, S. Yooseph, D. Allen, A. Basu, J. Baxendale, L. Blick, M. Caminha, J. Carnes-Stine, P. Caulk, Y.-H. Chiang, M. Coyne, C. Dahlke, A. D. Mays, M. Dombroski, M. Donnelly, D. Ely, S. Esparham, C. Fosler, H. Gire, S. Glanowski, K. Glasser, A. Glodek, M. Gorokhov, K. Graham, B. Gropman, M. Harris, J. Heil, S. Henderson, J. Hoover, D. Jennings, C. Jordan, J. Jordan, J. Kasha, L. Kagan, C. Kraft, A. Levitsky, M. Lewis, X. Liu, J. Lopez, D. Ma, W. Majoros, J. McDaniel, S. Murphy, M. Newman, T. Nguyen, N. Nguyen, M. Nodell, S. Pan, J. Peck, M. Peterson, W. Rowe, R. Sanders, J. Scott, M. Simpson, T. Smith, A. Sprague, T. Stockwell, R. Turner, E. Venter, M. Wang, M. Wen, D. Wu, M. Wu, A. Xia, A. Zandieh, and X. Zhu, "The Sequence of the Human Genome," *Science* (80-.)., vol. 291, no. 5507, p. 1304 LP-1351, Feb. 2001.
- [3] D. J. Lockhart, H. Dong, M. C. Byrne, M. T. Follettie, M. V Gallo, M. S. Chee, M. Mittmann, C. Wang, M. Kobayashi, H. Norton, and E. L. Brown, "Expression monitoring by hybridization to high-density oligonucleotide arrays," *Nat Biotech*, vol. 14, no. 13, pp. 1675–1680, Dec. 1996.
- [4] K. V Voelkerding, S. A. Dames, and J. D. Durtschi, "Next-Generation Sequencing: From Basic Research to Diagnostics," *Clin. Chem.*, vol. 55, no. 4, p. 641 LP-658, Mar. 2009.
- [5] F. Sanger, S. Nicklen, and A. R. Coulson, "DNA sequencing with chain-terminating inhibitors," *Proc. Natl. Acad. Sci. U. S. A.*, vol. 74, no. 12, pp. 5463–5467, Dec. 1977.
- [6] F. Sanger and A. R. Coulson, "A rapid method for determining sequences in DNA by primed synthesis with DNA polymerase," *J. Mol. Biol.*, vol. 94, no. 3, pp. 441–448, 1975.
- [7] J. Schmutz, J. Wheeler, J. Grimwood, M. Dickson, J. Yang, C. Caoile, E. Bajorek, S. Black, Y. M. Chan, M. Denys, J. Escobar, D. Flowers, D. Fotopulos, C. Garcia, M. Gomez, E. Gonzales, L. Haydu, F. Lopez, L. Ramirez, J. Retterer, A. Rodriguez, S. Rogers, A. Salazar, M. Tsai, and R. M. Myers, "Quality assessment of the human genome sequence," *Nature*, vol. 429, no. 6990, pp. 365–368, May 2004.
- [8] A. McKenna, M. Hanna, E. Banks, A. Sivachenko, K. Cibulskis, A. Kernytsky, K. Garimella, D. Altshuler, S. Gabriel, M. Daly, and M. A. DePristo, "The Genome Analysis Toolkit: A MapReduce framework for analyzing next-generation DNA sequencing data," *Genome Res.*, vol. 20, no. 9, pp. 1297–1303, Sep. 2010.
- [9] M. L. Metzker, "Sequencing technologies [mdash] the next generation," *Nat Rev Genet*, vol. 11, no. 1, pp. 31–46, Jan. 2010.
- [10] J. Shendure and H. Ji, "Next-generation DNA sequencing," *Nat Biotech*, vol. 26, no. 10, pp. 1135–1145, Oct. 2008.
- [11] E. R. Mardis, "Next-Generation Sequencing Platforms," *Annu. Rev. Anal. Chem.*, vol. 6, no. 1, pp. 287–303, Jun. 2013.
- [12] D. C. Koboldt, K. M. Steinberg, D. E. Larson, R. K. Wilson, and E. Mardis, "The Next-Generation Sequencing Revolution and Its Impact on Genomics," *Cell*, vol. 155, no. 1, pp. 27–38, Sep. 2013.

- [13] K. Wetterstrand, "DNA Sequencing Costs: Data from the NHGRI Genome Sequencing Program (GSP)." [Online]. Available: www.genome.gov/sequencingcostsdata.
- [14] T. Tucker, M. Marra, and J. M. Friedman, "Massively Parallel Sequencing: The Next Big Thing in Genetic Medicine," *Am. J. Hum. Genet.*, vol. 85, no. 2, pp. 142–154, Aug. 2009.
- [15] J. R. ten Bosch and W. W. Grody, "Keeping Up With the Next Generation: Massively Parallel Sequencing in Clinical Diagnostics," *J. Mol. Diagn.*, vol. 10, no. 6, pp. 484–492, Nov. 2008.
- [16] J. M. Rothberg, W. Hinz, T. M. Rearick, J. Schultz, W. Mileski, M. Davey, J. H. Leamon, K. Johnson, M. J. Milgrew, M. Edwards, J. Hoon, J. F. Simons, D. Marran, J. W. Myers, J. F. Davidson, A. Branting, J. R. Nobile, B. P. Puc, D. Light, T. a Clark, M. Huber, J. T. Branciforte, I. B. Stoner, S. E. Cawley, M. Lyons, Y. Fu, N. Homer, M. Sedova, X. Miao, B. Reed, J. Sabina, E. Feierstein, M. Schorn, M. Alanjary, E. Dimalanta, D. Dressman, R. Kasinskas, T. Sokolsky, J. a Fidanza, E. Namsaraev, K. J. McKernan, A. Williams, G. T. Roth, and J. Bustillo, "An integrated semiconductor device enabling non-optical genome sequencing.," *Nature*, vol. 475, no. 7356, pp. 348–352, 2011.
- [17] M. A. Quail, M. Smith, P. Coupland, T. D. Otto, S. R. Harris, T. R. Connor, A. Bertoni, H. P. Swerdlow, and Y. Gu, "A tale of three next generation sequencing platforms: comparison of Ion Torrent, Pacific Biosciences and Illumina MiSeq sequencers," *BMC Genomics*, vol. 13, no. 1, p. 341, 2012.
- [18] E. Pennisi, "Semiconductors Inspire New Sequencing Technologies," *Science* (80-.)., vol. 327, no. 5970, p. 1190 LP-1190, Mar. 2010.
- [19] L. Mamanova, R. M. Andrews, K. D. James, E. M. Sheridan, P. D. Ellis, C. F. Langford, T. W. Ost, J. E. Collins, and D. J. Turner, "FRT-seq: amplification-free, strand-specific transcriptome sequencing," *Nat Methods*, vol. 7, 2010.
- [20] N. Rusk, "Torrents of sequence," *Nat Meth*, vol. 8, no. 1, p. 44, Jan. 2011.
- [21] L.-T. Yin, J.-C. Chou, W.-Y. Chung, T.-P. Sun, and S.-K. Hsiung, "Separate structure extended gate H+-ion sensitive field effect transistor on a glass substrate," *Sensors Actuators B Chem.*, vol. 71, no. 1, pp. 106–111, 2000.
- [22] J. van der spiegel, I. Lauks, P. Chan, and D. Babic, "The extended gate chemically sensitive field effect transistor as multi-species microprobe," *Sensors and Actuators*, vol. 4, no. C, 1983.
- [23] P. D. Batista and M. Mulato, "ZnO extended-gate field-effect transistors as pH sensors," *Appl. Phys. Lett.*, vol. 87, no. 14, p. 143508, Sep. 2005.
- [24] S. M. Sze and K. K. Ng, *Physics of Semiconductor Devices*, 3rd ed. Wiley, 2006.
- [25] L. DeFrancesco, "Life Technologies promises [dollar]1,000 genome," *Nat Biotech*, vol. 30, no. 2, p. 126, Feb. 2012.

- [26] I. Heller, S. Chatoor, J. M??nnik, M. A. G. Zevenbergen, J. B. Oostinga, A. F. Morpurgo, C. Dekker, and S. G. Lemay, "Charge noise in graphene transistors," *Nano Lett.*, vol. 10, no. 5, pp. 1563–1567, 2010.
- [27] R. R. Harrison, "The Design of Integrated Circuits to Observe Brain Activity," *Proceedings of the IEEE*, vol. 96, no. 7. pp. 1203–1216, 2008.
- [28] C. G. Jakobson and Y. Nemirovsky, "I/f noise in ion sensitive field effect transistors from subthreshold to saturation," *IEEE Trans. Electron Devices*, vol. 46, no. 1, pp. 259–261, 1999.
- [29] A. Hassibi, R. Navid, R. W. Dutton, and T. H. Lee, "Comprehensive study of noise processes in electrode electrolyte interfaces," *J. Appl. Phys.*, vol. 96, no. 2, pp. 1074–1082, 2004.
- [30] M. J. Deen, M. W. Shinwari, J. C. Ranuárez, and D. Landheer, "Noise considerations in field-effect biosensors," *J. Appl. Phys.*, vol. 100, no. 7, pp. 74703–74708, 2006.
- [31] N. K. Rajan, D. A. Routenberg, J. Chen, and M. A. Reed, "1/f noise of silicon nanowire BioFETs," *IEEE Electron Device Lett.*, vol. 31, no. 6, pp. 615–617, 2010.
- [32] N. K. Rajan, D. A. Routenberg, and M. A. Reed, "Optimal signal-to-noise ratio for silicon nanowire biochemical sensors," *Appl. Phys. Lett.*, vol. 98, no. 26, pp. 2–4, 2011.
- [33] A. Tarasov, W. Fu, O. Knopfmacher, J. Brunner, M. Calame, and C. Schönenberger, "Signal-to-noise ratio in dual-gated silicon nanoribbon field-effect sensors," *Appl. Phys. Lett.*, vol. 98, no. 1, pp. 2011–2014, 2011.
- [34] J. Go, P. R. Nair, and M. A. Alam, "Theory of signal and noise in double-gated nanoscale electronic pH sensors," *J. Appl. Phys.*, vol. 112, no. 3, p. 34516, 2012.
- [35] D. Zhang, X. Gao, S. Chen, H. Norstr??m, U. Smith, P. Solomon, S. L. Zhang, and Z. Zhang, "An ion-gated bipolar amplifier for ion sensing with enhanced signal and improved noise performance," *Appl. Phys. Lett.*, vol. 105, no. 8, p. 82102, 2014.
- [36] K. Bedner, V. A. Guzenko, A. Tarasov, M. Wipf, R. L. Stoop, S. Rigante, J. Brunner, W. Fu, C. David, M. Calame, J. Gobrecht, and C. Schönenberger, "Investigation of the dominant 1/f noise source in silicon nanowire sensors," *Sensors Actuators, B Chem.*, vol. 191, pp. 270–275, 2014.
- [37] D. Zhang, I. Must, N. L. Netzer, X. Xu, P. Solomon, S. L. Zhang, and Z. Zhang, "Direct assessment of solid-liquid interface noise in ion sensing using a differential method," *Appl. Phys. Lett.*, vol. 108, no. 15, p. 151603, Apr. 2016.
- [38] J. Zhuge, R. Wang, R. Huang, Y. Tian, L. Zhang, D. W. Kim, D. Park, and Y. Wang, "Investigation of Low-Frequency Noise in Silicon Nanowire MOSFETs," *IEEE Electron Device Letters*, vol. 30, no. 1. pp. 57–60, 2009.
- [39] A. Haemmerli, J. Janata, and J. J. Brophy, "Equilibrium Noise in Ion Selective Field Effect Transistors," *J. Electrochem. Soc.*, vol. 129, no. 10, pp. 2306–2312, Oct. 1982.

- [40] P. R. Barabash and R. S. C. Cobbold, "Basic limitations of isfet and silicon pressure transducers: noise theory, models and device scaling," *Sensors and Actuators*, vol. 4, no. C, pp. 427–438, Jan. 1983.
- [41] M. V. Hauf, L. H. Hess, J. Howgate, M. Dankerl, M. Stutzmann, and J. A. Garrido, "Low-frequency noise in diamond solution-gated field effect transistors," *Appl. Phys. Lett.*, vol. 97, no. 9, 2010.
- [42] N. Clément, K. Nishiguchi, J. F. Dufreche, D. Guerin, A. Fujiwara, and D. Vuillaume, "A silicon nanowire ion-sensitive field-effect transistor with elementary charge sensitivity," *Appl. Phys. Lett.*, vol. 98, no. 1, pp. 1–4, 2011.
- [43] S. Chen, A. Van Den Berg, and E. T. Carlen, "Sensitivity and detection limit analysis of silicon nanowire bio(chemical) sensors," *Sensors Actuators, B Chem.*, vol. 209, pp. 486–489, 2015.
- [44] K. Georgakopoulou, A. Birbas, and C. Spathis, "Modeling of fluctuation processes on the biochemically sensorial surface of silicon nanowire field-effect transistors," *J. Appl. Phys.*, vol. 117, no. 10, 2015.
- [45] M. S. Crosser, M. A. Brown, P. L. McEuen, and E. D. Minot, "Determination of the Thermal Noise Limit of Graphene Biotransistors," *Nano Lett.*, vol. 15, no. 8, pp. 5404–5407, 2015.
- [46] R. L. Stoop, K. Thodkar, I. D. C. Molecular, U. De Valencia, C. Schönenberger, and M. Calame, "Charge Noise in Organic Electrochemical Transistors," *Phys. Rev. Appl.*, vol. 14009, pp. 1–8, 2017.
- [47] J. G. Webster and H. Eren, Measurement, instrumentation, and sensors handbook: electromagnetic, optical, radiation, chemical, and biomedical measurement. CRC press, 2014.
- [48] A. V. Der Ziel, "Theory of Shot Noise in Junction Diodes and Junction Transistors," *Proceedings of the IRE*, vol. 43, no. 11. pp. 1639–1646, 1955.
- [49] K. B. Oldham, "A Gouy-Chapman-Stern model of the double layer at a (metal)/(ionic liquid) interface," *J. Electroanal. Chem.*, vol. 613, no. 2, pp. 131–138, 2008.
- [50] O. Stern, "ZUR THEORIE DER ELEKTROLYTISCHEN DOPPELSCHICHT," Berichte der Bunsengesellschaft für Phys. Chemie, vol. 30, no. 21-22, pp. 508–516, 1924.
- [51] D. E. Yates, S. Levine, and T. W. Healy, "Site-binding model of the electrical double layer at the oxide/water interface," *J. Chem. Soc. Faraday Trans. 1 Phys. Chem. Condens. Phases*, vol. 70, no. 0, p. 1807, 1974.
- [52] L. Bousse, L. Bousse, N. F. De Rood, and P. Bergveld, "Operation of Chemically Sensitive Field-Effect Sensors As a Function of the Insulator-Electrolyte Interface," *IEEE Trans. Electron Devices*, vol. 30, no. 10, pp. 1263–1270, 1983.
- [53] R. E. G. van Hal, J. C. T. Eijkel, and P. Bergveld, "A general model to describe the electrostatic potential at electrolyte oxide interfaces," *Adv. Colloid Interface Sci.*, vol. 69, no. 1–3, pp. 31–62, 1996.

- [54] J. B. Johnson, "Thermal Agitation of Electricity in Conductors," *Phys. Rev.*, vol. 32, no. 1, pp. 97–109, Jul. 1928.
- [55] H. Nyquist, "Thermal Agitation of Electric Charge in Conductors," *Phys. Rev.*, vol. 32, no. 1, pp. 110–113, Jul. 1928.
- [56] R. Kubo, "The fluctuation-dissipation theorem," *Reports Prog. Phys.*, vol. 29, no. 1, p. 255, 1966.
- [57] A. J. Bard and L. R. Faulkner, *Electrochemical Methods; Fundamentals and Applications*, 2nd ed. Wiley, 2001.
- [58] M. R. Shoar Abouzari, F. Berkemeier, G. Schmitz, and D. Wilmer, "On the physical interpretation of constant phase elements," *Solid State Ionics*, vol. 180, no. 14–16, pp. 922–927, 2009.
- [59] G. J. Brug, A. L. G. van den Eeden, M. Sluyters-Rehbach, and J. H. Sluyters, "The analysis of electrode impedances complicated by the presence of a constant phase element," *J. Electroanal. Chem.*, vol. 176, no. 1–2, pp. 275–295, 1984.
- [60] G. Láng and K. E. Heusler, "Remarks on the energetics of interfaces exhibiting constant phase element behaviour," *J. Electroanal. Chem.*, vol. 457, no. 1–2, pp. 257–260, Feb. 1998.
- [61] J. R. Mcdonald, *Impedance spectroscopy: emphasizing solid materials and systems*. Wiley, 1987.
- [62] R. L. Hurt and J. R. Macdonald, "Distributed circuit elements in impedance spectroscopy: A unified treatment of conductive and dielectric systems," *Solid State Ionics*, vol. 20, no. 2, pp. 111–124, 1986.
- [63] W. H. Mulder, J. H. Sluyters, T. Pajkossy, and L. Nyikos, "Tafel current at fractal electrodes. Connection with admittance spectra," *J. Electroanal. Chem.*, vol. 285, no. 1–2, pp. 103–115, 1990.
- [64] U. Rammelt and G. Reinhard, "On the applicability of a constant phase element (CPE) to the estimation of roughness of solid metal electrodes," *Electrochim. Acta*, vol. 35, no. 6, pp. 1045–1049, 1990.
- [65] Z. Kerner, "Impedance of rough capacitive electrodes: the role of surface disorder," *J. Electroanal. Chem.*, vol. 448, no. 1, pp. 139–142, 1998.
- [66] J. Vogelsang and W. Strunz, "The evaluation of experimental dielectric data of barrier coatings by means of different models," *Electrochim. Acta*, vol. 46, no. 24–25, pp. 3619–3625, 2001.
- [67] T. Pajkossy, "Impedance spectroscopy at interfaces of metals and aqueous solutions Surface roughness, CPE and related issues," *Solid State Ionics*, vol. 176, no. 25–28, pp. 1997–2003, 2005.
- [68] S. M. George, "Atomic layer deposition: An overview," *Chem. Rev.*, vol. 110, no. 1, pp. 111–131, Jan. 2010.
- [69] C. Hitz and A. Lasia, "Experimental study and modeling of impedance of the her on porous Ni electrodes," *J. Electroanal. Chem.*, vol. 500, no. 1–2, pp. 213–222, 2001.
- [70] J.-B. Jorcin, M. E. Orazem, N. Pébère, and B. Tribollet, "CPE analysis by local electrochemical impedance spectroscopy," *Electrochim. Acta*, vol. 51, no. 8–9, pp. 1473–1479, 2006.

- [71] K. B. Oldham, "The RC time 'constant' at a disk electrode," *Electrochem. commun.*, vol. 6, no. 2, pp. 210–214, 2004.
- [72] A. K. Jonscher, "Dielectric relaxation in solids," *J. Phys. D. Appl. Phys.*, vol. 32, no. 14, pp. R57–R70, 1999.
- [73] L. Young, "Anodic oxide films. Part 4.?The interpretation of impedance measurements on oxide coated electrodes on niobium," *Trans. Faraday Soc.*, vol. 51, no. 0, p. 1250, 1955.
- [74] M. Bojinov, G. Fabricius, T. Laitinen, T. Saario, and G. Sundholm, "Conduction mechanism of the anodic film on chromium in acidic sulphate solutions," *Electrochim. Acta*, vol. 44, no. 2–3, pp. 247–261, 1998.
- [75] B. Hirschorn, M. E. Orazem, B. Tribollet, V. Vivier, I. Frateur, and M. Musiani, "Determination of effective capacitance and film thickness from constant-phase-element parameters," *Electrochim. Acta*, vol. 55, no. 21, pp. 6218–6227, 2010.
- [76] B. Hirschorn, M. E. Orazem, B. Tribollet, V. Vivier, I. Frateur, and M. Musiani, "Constant-Phase-Element Behavior Caused by Resistivity Distributions in Films: I. Theory," *J. Electrochem. Soc.*, vol. 157, no. 12, pp. C452–C457, 2010.
- [77] P.-C. Yao, J.-L. Chiang, and M.-C. Lee, "Application of sol-gel TiO2 film for an extended-gate H+ ion-sensitive field-effect transistor," *Solid State Sci.*, vol. 28, pp. 47–54, 2014.
- [78] C. Jimenez-Jorquera, J. Orozco, and A. Baldi, "ISFET based microsensors for environmental monitoring," *Sensors*, vol. 10, no. 1, pp. 61–83, Jan. 2010.
- [79] Y.-H. Liao and J.-C. Chou, "Preparation and characterization of the titanium dioxide thin films used for pH electrode and procaine drug sensor by sol–gel method," *Mater. Chem. Phys.*, vol. 114, no. 2, pp. 542–548, 2009.
- [80] Y. Liu, P. Georgiou, T. Prodromakis, T. G. Constandinou, and C. Toumazou, "An extended CMOS ISFET model incorporating the physical design geometry and the effects on performance and offset variation," *IEEE Trans. Electron Devices*, vol. 58, no. 12, pp. 4414–4422, 2011.
- [81] Y. Wang, H. Yuan, X. Lu, Z. Zhou, and D. Xiao, "All solid-state pH electrode based on titanium nitride sensitive film," *Electroanalysis*, vol. 18, no. 15, pp. 1493–1498, 2006.
- [82] R. C. Gesteland, J. Y. Lettvin, B. Howland, B. Howland, and W. H. Pitts, "Comments on Microelectrodes," *Proc. IRE*, vol. 47, no. 11, pp. 1856–1862, 1959.
- [83] G. Láng and K. E. Heusler, "Remarks on the energetics of interfaces exhibiting constant phase element behaviour," *J. Electroanal. Chem.*, vol. 457, no. 1–2, pp. 257–260, 1998.
- [84] H. Achour, R. Talmat, B. Cretu, J. M. Routoure, A. Benfdila, R. Carin, N. Collaert, E. Simoen, A. Mercha, and C. Claey, "DC and low frequency noise performances of SOI p-FinFETs at very low temperature," *Solid. State. Electron.*, vol. 90, pp. 160–165, 2013.

- [85] E. Simoen, A. Veloso, Y. Higuchi, N. Horiguchi, and C. Claeys, "On the oxide trap density and profiles of 1-nm eot metal-gate last cmos transistors assessed by low-frequency noise," *IEEE Trans. Electron Devices*, vol. 60, no. 11, pp. 3849–3855, 2013.
- [86] C. G. Theodorou, E. G. Ioannidis, F. Andrieu, T. Poiroux, O. Faynot, C. A. Dimitriadis, G. Ghibaudo, and S. Member, "Low-Frequency Noise Sources in Advanced," vol. 61, no. 4, pp. 1161–1167, 2014.
- [87] D. V. Potapenko, G. T. Gomes, and R. M. Osgood, "Correlation of H Adsorption Energy and Nanoscale Elastic Surface Strain on Rutile TiO2(110)," *J. Phys. Chem. C*, vol. 120, no. 38, pp. 21373–21380, Sep. 2016.
- [88] J.-C. Chou and L. P. Liao, "Study on pH at the point of zero charge of TiO2 pH ion-sensitive field effect transistor made by the sputtering method," *Thin Solid Films*, vol. 476, no. 1, pp. 157–161, 2005.
- [89] P. W. Schindler and H. Gamsjäger, "Acid base reactions of the TiO2 (Anatase) water interface and the point of zero charge of TiO2 suspensions," *Kolloid-Zeitschrift Zeitschrift für Polym.*, vol. 250, no. 7, pp. 759–763, 1972.
- [90] M. Ashida, M. Sasaki, H. Kan, T. Yasunaga, K. Hachiya, and T. Inoue, "Kinetics of proton adsorption-desorption at TiO2-H2O interface by means of pressure-jump technique," *J. Colloid Interface Sci.*, vol. 67, no. 2, pp. 219–225, 1978.
- [91] H. Tamura, K. Mita, A. Tanaka, and M. Ito, "Mechanism of hydroxylation of metal oxide surfaces," *J. Colloid Interface Sci.*, vol. 243, no. 1, pp. 202–207, 2001.

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